Quantitative and localized spectroscopy for non-invasive bilirubinometry in neonates
Bosschaart, N.

Citation for published version (APA):
Bosschaart, N. (2012). Quantitative and localized spectroscopy for non-invasive bilirubinometry in neonates

General rights
It is not permitted to download or to forward/distribute the text or part of it without the consent of the author(s) and/or copyright holder(s), other than for strictly personal, individual use, unless the work is under an open content license (like Creative Commons).

Disclaimer/Complaints regulations
If you believe that digital publication of certain material infringes any of your rights or (privacy) interests, please let the Library know, stating your reasons. In case of a legitimate complaint, the Library will make the material inaccessible and/or remove it from the website. Please Ask the Library: http://uba.uva.nl/en/contact, or a letter to: Library of the University of Amsterdam, Secretariat, Singel 425, 1012 WP Amsterdam, The Netherlands. You will be contacted as soon as possible.
CHAPTER 7

Improved acquisition speed in low-coherence spectroscopy by means of spectroscopic detection

Low-coherence spectroscopy (LCS) is a promising technique for the non-invasive determination of blood composition, but its clinical utility may be limited by the speed of the current time domain detection scheme. In this Chapter, we investigate the possibility of spectroscopic detection in LCS (sdLCS), which has a theoretical sensitivity and/or speed advantage compared to time domain detection (tdLCS).

Since sdLCS requires the acquisition of spectra with both high spectral, and high spatial resolution, a new method of acquisition and analysis was developed. In this Chapter, we validate our method computationally in a simulation and experimentally on a phantom with known optical properties. The attenuation, absorption and scattering coefficient spectra from the phantom that were measured by sdLCS agree well with the expected optical properties and are comparable to the measured optical properties by tdLCS.
7.1 Introduction

In the previous Chapters 4 to 6, we have shown that low-coherence spectroscopy (LCS) can be used to measure local absorption, scattering and backscattering coefficient spectra in turbid media over almost the complete visible wavelength range (480 to 700 nm) [1-3]. By deriving hemoglobin concentrations from absorption coefficient spectra in the dermal microcirculation (Chapter 6), we showed that LCS is a promising technique for the localized quantification of tissue chromophore concentrations, which may lead to e.g. a non-invasive alternative for invasive blood sampling [3]. However, since most clinical applications require fast measurements for instantaneous diagnosis and the reduction of motion artifacts, the measurement speed of the current time domain LCS (tdLCS) system may limit its clinical applicability. From optical coherence tomography (OCT) studies, we know that spectroscopic detection allows for more sensitive measurements compared to time domain detection [4,5], which can be exchanged for higher acquisition speed at unaltered sensitivity. Therefore, in this Chapter we investigate the possibility for spectroscopic detection in LCS (sdLCS), focusing primarily on validating a new method of analysis that was developed for this purpose.

Spectroscopic detection in OCT commonly involves spectrographs with high spectral resolution, a narrow wavelength range and a large number of pixels, resulting in large effective imaging depths (i.e. high maximal imaging depth and weak sensitivity roll-off in depth). Consequently, an A-scan of several mm can be recovered from a single back scattered spectrum, which is used for constructing an intensity image with high spatial resolution [4,5]. In LCS, we are mainly interested in the spectral content of the signal within a confined volume and hence, LCS requires both high spatial and sufficient spectral resolution (Chapter 4). In the case of spectroscopic detection, this can be achieved either by signal processing after acquisition [6], or by adjusting the signal acquisition itself. Since the latter has not been investigated before, we developed a new approach for signal acquisition in sdLCS.

Our approach involves step-wise detection of local back scattered spectra with a spectrograph that has an effective imaging depth of only 9 μm in air. Thereby, we achieve both high spatial and sufficient spectral resolution (6 nm) and we maintain the advantage of focus tracking, as we had in our tdLCS system. The main challenge in step-wise spectroscopic detection with limited imaging depth involves removing the mirror image that originates from the complex ambiguity of the LCS signal. Methods for mirror image removal in OCT imaging commonly involve phase modulation and filtering of the modulated signal [8-10]. Similarly, our approach is to modulate the LCS signal, by using an oscillating mirror in the reference arm.

Since the primary aim of this Chapter is to validate whether we can use this new approach for the determination of local absorption and scattering coefficient spectra, we will provide proof of principle with an on-the-shelf spectrograph (USB4000, Ocean Optics, USA). Only part of the feasible speed advantage is demonstrated, since the quantum efficiency and acquisition speed of this spectrograph are not optimized for sdLCS. After describing the theory behind sdLCS, we will validate our algorithm with a simulation of an sdLCS absorption measurement, while simulating the USB4000 as the detecting spectrograph. Subsequently, we experimentally demonstrate the ability of
sdLCS to measure the attenuation, absorption and scattering coefficient spectra from a polystyrene-dye phantom, and we compare our results to a tdLCS measurement.

7.2 Theory

The main difference between sdLCS and tdLCS, is that the detector current $i_0$ is acquired as a function of wavelength $\lambda$ (e.g. by a spectrograph), instead of time by a photodiode (Chapters 4 to 6). Similar Eq. 4.1 for tdLCS, $i_0$ is modulated by the path length difference between the sample arm and the reference arm $\Delta L = 2(x_s - x_r)$, with sample arm length $x_s$ and reference arm length $x_r$. Hence, for sdLCS we can write:

$$\begin{align*}
    i_0(k) &\propto I_s(k) + I_r(k) + \sqrt{I_s(k) \cdot I_r(k)} \cdot 2\cos(k\Delta L) \\
    \text{where } k &\text{ is the wavenumber } (k = 2\pi/\lambda) \text{ and } I_s \text{ and } I_r \text{ are the signal intensities in the sample and reference arm, respectively. The two left terms of Eq. 7.1 denote the ('DC') non-modulated part of } i_0(k) \text{ and the right term denotes the ('AC') modulated part of } i_0(k), \text{ as has been illustrated in Figure 7.1a. Since } I_s \text{ and } I_r \text{ both originate from the source spectrum } S_0, \text{ the modulation term in Eq. 7.1 can be written in terms of } S_0. \text{ In case of a single reflector at path length } \ell \text{ (depth } \ell/2), \text{ this results in:}
\end{align*}$$

$$i_{0,\text{modulated}}(k) \propto \sqrt{\eta_s \cdot \eta_r \cdot e^{\mu t} \cdot S_0(k)} \cdot 2\cos(k\Delta L) \quad (7.2)$$

with $\eta_s$ and $\eta_r = 1-\eta_s$ the fractions of $S_0$ that are guided towards the sample and reference arm, respectively, as determined by the splitting ratio of the beam splitter. The light originating from the sample arm is backscattered by a sample with an attenuation coefficient $\mu_t$ and hence, $I_s$ is attenuated by Beer’s law if the geometrical path length $\ell$ in the sample increases. In sdOCT, an A-scan (i.e. the backscattered intensity as a function of $d = \mu t \Delta L$) is obtained by Fourier transformation of $i_0(k)$:

$$i_0(\Delta L) = \left| \mathcal{F}\{i_0(k)\} \right|^2 \quad (7.3)$$

As illustrated in Figure 7.1b, the horizontal axis of $i_0(\Delta L)$ runs from $-\Delta L_{\text{max}}$ to $\Delta L_{\text{max}}$. For every $\Delta L$ a ‘mirror image’ is present at $-\Delta L$, i.e. both these path length differences result in the same modulation frequency on $i_0(k)$ (Eq. 7.1 and 7.2). The Nyquist criterion defines the maximal measurable path length difference $\Delta L_{\text{max}}$ or imaging depth $d_{\text{max}} = \mu t \Delta L_{\text{max}}$:

$$\Delta L_{\text{max}} = \frac{\pi}{\delta k} \quad (7.4)$$

in which $\delta k = (k_{\text{max}} - k_{\text{min}})/N_p$ depends entirely on the properties of the detecting spectrograph, which are the number of pixels $N_p$, and the minimal and maximal detectable wave number $k_{\text{min}}$ and $k_{\text{max}}$.

The path length range over which $I(\Delta L)$ can be observed not only depends on $\Delta L_{\text{max}}$, but also on the sensitivity roll-off with $\Delta L$ of the spectrograph, caused by the finite spectrometer resolution [11]:
in which $\Delta k$ is the spectral resolution of the spectrograph.

Since we use sdLCS for doing spectroscopy, we are interested in the spectrum $i_0(k)$ itself, rather than an A-scan as in sdOCT. However, Eq. 7.4 and 7.5 are important for sdLCS, since the $\Delta l_{\text{max}}$ and the signal roll-off determine the highest measurable modulation frequency in $i_0(k)$, and therefore the spatial resolution at which the spectrum $i_0(k)$ can be acquired. In contrast to sdOCT, sdLCS requires low values of $\Delta l_{\text{max}}$ and a fast sensitivity roll-off to obtain good spatial resolution for $i_0(k)$ (see Section 7.4). Similar to tdLCS, this introduces a trade-off between the spectral and spatial resolution of $i_0(k)$, because a fast sensitivity roll-off is accompanied by a low spectral resolution $\Delta k$ (Eq. 7.5).

### 7.2.1 Mirror image removal

Merely acquiring $i_0(k)$ within a confined path length range does not provide us with a spectrum that we can use for the determination of $\mu_v$ since $i_0(k)$ contains unwanted DC (i.e. non-modulated components) and modulation components (Eq. 7.1 and 7.2). Moreover, the mirror image induces cross-talk between $i_0(\Delta l)$ and $i_0(-\Delta l)$ within the investigated path length range. This complex ambiguity can be removed by phase modulation and frequency domain filtering of the signal. Therefore, we modulate $i_0(k)$ using the oscillating mirror in the reference arm of our LCS system, which introduces a Doppler shift $f_0$ to the signal:

$$f_0 = \frac{2v_r}{\lambda} = \frac{v_r \cdot k}{\pi}$$

with $v_r$ the velocity of the reference mirror. Acquisition of N spectra $i_0(k)$ at every integration time $\tau$ of the spectrograph results in a dataset $i_0(k,t)$, as illustrated in Figure 7.1c. The phase of the modulation on $i_0(k,t)$ changes at every $\tau$, because the movement of the reference mirror induces a change in $\Delta l$ (vertical direction in Figure 7.1c). Figure 7.1d illustrates the time-modulation on $i_0(k,t)$ by $f_0$ for one wavelength (horizontal direction in Figure 7.1c). Since the sensitivity of the measurement is largest around $\Delta l = 0$ or ‘zero delay’ (Eq. 7.5), the range of $\Delta l$ is chosen such that it crosses zero delay at $\approx N \tau$ (Figure 7.1e). The integration time of the spectrograph should be chosen such that the time-modulation on $i_0(k,t)$ is adequately sampled. Hence the sampling frequency $f_s = 1/\tau$ needs to be larger than $2f_{0,\text{max}}$ (the largest value of $f_0$ within the investigated spectral range). For the integration time, this results in:

$$\tau < \frac{\pi}{2v_r \cdot k_{\text{max}}} = \frac{\lambda_{\text{min}}}{4v_r}$$

with $k_{\text{max}}$ the largest wave number and $\lambda_{\text{min}}$ the shortest wavelength within the investigated spectral range.

Fourier transformation on $i_0(k,t)$ with respect to $t$ provides the frequency content of the signal $i_0(k,f)$, which contains the modulation frequency $f_0$, its mirror image and a DC component (Figure 7.1f). By filtering out the part of $i_0(k,f)$ containing only the positive
frequencies $+f_o$, the unwanted DC component and the negative frequencies $-f_o$ are lost. Now that $i_0(k)$ is confined both in amplitude and phase, the complex ambiguity and the mirror image in the path length domain (Figure 7.1b) are lost. Inverse Fourier transformation on the filtered $i_0(k,f)$ with respect to $f$ provides a smooth, non-modulated $i_0(k,t)$ (Figure 7.1g), and averaging of $i_0(k,t)$ over time results in the final spectrum $S$ that we can use for the determination of $\mu_t$ (Figure 7.1h).

Similar to tdLCS, a dataset $S(\xi)$ is generated by step-wise alteration of the depth or geometrical round trip path length $\xi$ in the sample around which $i_0(k)$ is acquired (Chapter 4). Hence, the advantage of focus tracking that we had in tdLCS can still be applied in sdLCS.

### 7.2.2 Sensitivity and/or speed advantage

Our method for sdLCS provides a sensitivity advantage over tdLCS, which can be explained in terms of the signal to noise ratio (SNR). The SNR of any shot-noise limited LCS system is given by:

$$ SNR = \frac{\varepsilon \cdot S}{h \nu \cdot \Delta f} \tag{7.8} $$

in which $\varepsilon$ is the detection efficiency, $h \nu$ the photon energy and $\Delta f$ the detection bandwidth of the system [5]. Using Eq. 4.8, we can write:

$$ \Delta f = 2f_{scan} d_{scan} \frac{\lambda}{\lambda_0^2} \tag{7.9} $$

with $f_{scan}$ the scan rate and $d_{scan}$ the scan length for the acquisition of one spectrum. For tdLCS, $f_{scan}=2f_R$ and $d_{scan}=\Delta R$ (Chapter 4). For sdLCS, $f_{scan}=1/\tau$ and $d_{scan}=2d_{max} = \Delta L_{max} = \lambda^2/(2\Delta \lambda)$, if mirror image removal is applied. If we assume that in sdLCS, $N_p$ pixels cover the bandwidth of the spectrum $S$, i.e. $N_p \cdot \delta \lambda = \Delta \lambda$, then $d_{scan}$ can be written into $d_{scan} = \frac{N_p \lambda^2}{2\Delta \lambda}$. Hence for sdLCS, $\Delta f$ reduces to $\Delta f = N_p f_{scan}$. As a consequence, the SNR of a tdLCS system compares to the SNR of an sdLCS system as $SNR_{TD} = (\varepsilon \cdot S)/(h \nu \cdot \Delta f) = (\tau \cdot \varepsilon \cdot S)/(h \nu N_p f_{scan}) = SNR_{SD}/N_p$. In conclusion, sdLCS is $N_p$-times more sensitive than tdLCS, provided that both systems have the same $f_{scan}$, $d_{scan}$ and $\varepsilon$. This sensitivity advantage can be exchanged for a speed advantage if $f_{scan}$ is increased, i.e. an sdLCS system can measure $N_p$-times faster than a tdLCS system with equal sensitivity.

A change in $f_{scan}$ - i.e. between a ‘fast’ and a ‘slow’ LCS system - results in an SNR change with a factor $\phi = \Delta f_{slow}/\Delta f_{fast} = (f_{scan,fast} d_{scan,fast})/(f_{scan,slow} d_{scan,slow})$, which comprises $\phi = 2f_R \tau (\Delta R/\Delta L_{max})$ for a ‘fast’ system with the sdLCS settings (but without spectral detection) and a ‘slow’ system with the tdLCS settings. If in addition, spectral detection over $N_p$ pixels is realized for the ‘fast’ system (as for our sdLCS system), the SNR will increase with a factor $N_p$. As a consequence, the SNR$_{SD}$ of an sdLCS system relates to the SNR$_{TD}$ of a tdLCS system as:

$$ SNR_{SD} = \phi \cdot N_p \cdot \frac{\varepsilon_{SD}}{\varepsilon_{TD}} \cdot SNR_{TD} = 2f_R \cdot \tau \cdot N_p \cdot \frac{\varepsilon_{SD}}{\varepsilon_{TD}} \cdot \frac{\Delta R}{\Delta L_{max}} \cdot SNR_{TD} \tag{7.10} $$

which also considers a possible difference in detection efficiency between sdLCS and tdLCS.
Figure 7.1: Signal acquisition and processing in sdLCS. See Section 7.2 for details.
7.3 Simulation

In order to validate the data acquisition and analysis approach described in Section 7.2, we simulated an absorption measurement on a sample containing oxyhemoglobin [12]. Since scattering was neglected in the simulation, the attenuation coefficient $\mu_\text{s}$ in Eq. 7.2 can be simplified to the absorption coefficient $\mu_a$. The spectrum $S(\ell)$ was calculated at $\ell_1 = 2$ mm and $\ell_2 = 4$ mm inside the sample, corresponding to depths $d_1 = 1$ mm and at $d_2 = 2$ mm, respectively.

The detecting spectrograph was simulated with the properties of the USB4000 ($\lambda_{\text{min}} = 345$ nm, $\lambda_{\text{max}} = 1042$ nm, $N_p = 3648$). The integration time was set at the minimal integration time of the USB4000 for these measurements, $\tau = 6$ ms. To meet the requirement in Eq. 7.7, the velocity of the reference mirror was set at $v_R = 6$ $\mu$m/s (frequency $f_R = 0.3$ Hz, amplitude $\Delta R = 20$ $\mu$m). The source spectrum $S_\text{o}$ was simulated as a Gaussian with center wavelength $\lambda_0 = 550$ nm and bandwidth $\lambda_{\text{FWHM}} = 140$ nm. The sample arm fraction was $\eta_s = 0.1$, resulting in a reference arm fraction of $\eta_R = 0.9$. A total number of $N = 125$ spectra was acquired over a time interval of $N\tau = 0.75$ s. The initial $\Delta L$ was set at -4.5 $\mu$m to achieve zero delay at $\frac{1}{2}N\tau$.

Figure 7.2 shows the result of this simulation. The $i_0(\lambda)$ at $\ell_1$ and $\ell_2$ show little influence of the sample’s absorption (Figure 7.2a). However, after phase modulation and frequency domain filtering of $i_0(\lambda)$, the resulting spectra $S$ at $\ell_1$ and $\ell_2$ clearly show the presence of the oxyhemoglobin absorption peaks (Figure 7.2b). Using Beer’s law, we obtain the absorption coefficient of the sample:

$$\mu_a = -\frac{1}{\frac{1}{2}(\ell_2 - \ell_1)} \ln \left( \frac{S(\ell_2)}{S(\ell_1)} \right)$$

(7.11)

From Figure 7.2c, we can conclude that our method of data acquisition and analysis for sdLCS fully recovers the input $\mu_a$ of this simulation.

![Figure 7.2 Simulation of a $\mu_a$ measurement in sdLCS. a.) input spectra $i_0$ and b.) filtered spectra $S$ at path lengths $\ell_1$ and $\ell_2$ inside the sample. c.) input $\mu_a$ and recovered $\mu_a$ from Eq. 7.8.](image)
7.4 The path length window $\Delta \ell$ in sdLCS

In sdLCS, the path length window over which $S(\ell)$ is acquired depends not only on the reference mirror scanning window in the medium ($\Delta \ell_R = 2\Delta R/n_g = 30 \mu m$ with the settings of Section 7.3 and group refractive index $n_g = 1.35$), but also on the path length window that is probed by the spectrograph $\Delta \ell_S$. The latter is a combination of $2\Delta L_{\text{max}}$ (due to mirror image removal) and the sensitivity roll-off with $\Delta L$ of the spectrograph. For the USB4000, we can calculate that $2\Delta L_{\text{max}} = 1880 \mu m$ (Eq. 7.4), but its sensitivity roll-off is not readily available.

To determine the sensitivity roll-off of the USB4000, we both calculated (Eq. 7.5) and measured its roll-off function. Since the only unknown parameter in Eq. 7.5 is the spectral resolution $\Delta k$ (or $\Delta \lambda = 2\pi/\Delta k$), we measured $\Delta \lambda = 6 \text{ nm}$ as the FWHM of a 543 nm and 633 nm HeNe laser line, projected on the spectrograph. This spectral resolution results in a theoretical sensitivity roll-off with a FWHM of 18 um, indicated by the dotted line in Figure 7.3.

We experimentally determined the sensitivity roll-off by measuring the reflection from a glass slide in the sample arm as a function of $\Delta L$ between the sample arm and the reference arm, using Eq. 7.3. The measured $i_0(\lambda)$ was resampled to a linear $k$-scale. The resulting sensitivity roll-off function is shown in Figure 7.3 and agrees very well with the theoretical function. Note that the width (FWHM) of the reflections at each value of $\Delta L$ is close to twice the coherence length ($2\cdot\ell_c = 3 \mu m$, Eq. 4.4) of the source (identical to the source in Chapters 4 to 6), and therefore agrees with the theoretical resolution for $\Delta L$.

Since the FWHM of the sensitivity roll-off of the USB4000 is 18 um, which is many times smaller than the $2\Delta L_{\text{max}}$ of 1880 um, the path length window that is probed by the USB4000 can be approximated with $\Delta \ell_S = 18/n_g = 13 \mu m$. This $\Delta \ell_S$ probes a path length window around every path length $\ell$ in the reference mirror scanning window $\Delta \ell_R$. Hence, the full path length window that is probed in sdLCS is a convolution of $\Delta \ell_R$ with $\Delta \ell_S$, resulting in $\Delta \ell = \Delta \ell_R + \Delta \ell_S = 30 + 13 = 43 \mu m$ (inset of Figure 7.3).

![Figure 7.3](image_url)
7.5 Experimental validation – Methods

To experimentally validate our approach for sdLCS (Section 7.2), we measured attenuation spectra $\mu_t$ from 480 to 700 nm on a phantom with known absorption $\mu_a$ and scattering $\mu_s$ coefficient spectra and we separated the individual contributions of $\mu_a$ and $\mu_s$ from the measured $\mu_t$. In addition, we compared our sdLCS results to the results of a tdLCS measurement on the same phantom with the tdLCS system described in Chapters 4 to 6 (Figure 4.1) [1-3].

*Table 7.1 Acquisition settings for sdLCS and tdLCS*

<table>
<thead>
<tr>
<th>acquisition parameter</th>
<th>sdLCS</th>
<th>tdLCS</th>
</tr>
</thead>
<tbody>
<tr>
<td>$\Delta \ell$</td>
<td>43 $\mu$m</td>
<td>44 $\mu$m</td>
</tr>
<tr>
<td>$\Delta \lambda$</td>
<td>6 nm (all $\lambda$)</td>
<td>4 nm @ $\lambda$=480 nm</td>
</tr>
<tr>
<td>$\nu_R$</td>
<td>0.006 mm/s</td>
<td>1.84 mm/s</td>
</tr>
<tr>
<td>$f_R$</td>
<td>0.3 Hz</td>
<td>23 Hz</td>
</tr>
<tr>
<td>$\Delta R$</td>
<td>20 $\mu$m</td>
<td>40 $\mu$m</td>
</tr>
<tr>
<td>N = # averages per $\ell$</td>
<td>250</td>
<td>250</td>
</tr>
<tr>
<td>acquisition time of $S(\ell)$</td>
<td>$N\tau = 1.5$ s</td>
<td>$N/(2f_R) = 5.4$ s</td>
</tr>
</tbody>
</table>

7.5.1 System and acquisition

The sdLCS system described in this Chapter is identical to the tdLCS system in Chapters 4 to 6, except for the detection end of the system, which consists of a spectrograph rather than a photodiode/lock-in amplifier combination. Hence, the multimode detection fiber is connected to the detecting spectrograph (USB4000), from which the properties have been described in Section 7.3.

For both the sdLCS and tdLCS measurements, we controlled $\ell$ ($\ell = 0 – 2000$ $\mu$m) by translating the reference mirror in steps of 27 $\mu$m. By translating the sample in the axial direction, focus tracking of the spot size ($r = 4.5$ $\mu$m) in the medium was achieved. At every $\ell$, back scattered power spectra $S(\ell)$ were obtained over a path length window in the medium of $\Delta \ell = 43$ $\mu$m for sdLCS (see Sections 7.2 and 7.4) and $\Delta \ell = 44$ $\mu$m for tdLCS (see Chapter 4). For both sdLCS and tdLCS, $S(\ell)$ was temporally averaged (N = 250 spectra per $\ell$) and corrected for the background (i.e. the LCS spectrum obtained from the non-scattering glass of the inner cuvette wall of the sample). The integration time for the sdLCS measurements was set at $\tau = 6$ ms and the reference mirror velocity at $\nu_R = 6$ $\mu$m/s, identical to the settings of the simulation (Section 7.3). The acquisition
settings for the tdLCS measurements were identical to the settings in Chapters 4 to 6 [1-3]. For both sdLCS and tdLCS, the most important acquisition parameters have been summarized in Table 7.1. Note that the acquisition speed for one temporally averaged spectrum \( S(\ell) \) is 3.6 times faster for sdLC.

Similar to the data analysis in Chapters 4 to 6, fitting the single exponential decay model \( S(\ell) = \alpha \exp(-\mu_a \ell) \) (free running fit parameters \( \alpha \) and \( \mu_a \)) to the sdLC and tdLC acquired \( S(\ell) \) vs. \( \ell \), results in a \( \mu_s \) spectrum for both detection methods [1-3]. Uncertainties in \( \alpha \) and \( \mu_a \) are estimated by their 95% confidence intervals (c.i.). Since the spectral resolution in sdLC (\( \Delta \lambda = 6 \text{ nm} \), Section 7.4) is higher than the pixel width of 0.2 nm, \( S(\ell) \) was binned into wavelength regions of 6 nm for the sdLC measurements. The values of \( \mu_s \) and \( \mu_a \) were obtained by fitting their individual contributions to the measured \( \mu_a \), as described in Chapter 6.2.2 [3].

### 7.5.2 Phantom

We prepared one phantom, consisting of 0.096 vol% NIST-certified polystyrene spheres (\( \Phi \ 602\pm6 \text{ nm} \), Thermo Scientific, USA) and 10% magenta dye (Ecoline #337, Royal Talens, The Netherlands). The \( \mu_s \) of the polystyrene spheres was calculated using Mie theory and integrated over the size distribution of the spheres (2\( \times \)SD), as described in Chapter 5.2.4 [2]. The \( \mu_s \) of the dye was determined in a separate transmission measurement on the dye only, as described in Chapter 4.3.2 [1]. For the tdLC measurements, both reference spectra for \( \mu_a \) and \( \mu_s \) were convolved with a Lorentzian with a line width of 9 nm for adequate comparison to the LCS spectra that are Doppler broadened by Brownian motion (Chapters 4 to 6) [1-3]. For the sdLC measurements, Brownian motion does not induce spectral broadening, because the Doppler shifted frequencies are still within the bounds of the frequency domain filter (Figure 7.1f). Since the reference spectrum of \( \mu_s \) was obtained with the same spectral resolution as the LCS spectra, we did not broaden this spectrum. The reference spectrum of \( \mu_s \) was convolved with a Lorentzian with a line width of 6 nm (\( \Delta \lambda \) of the USB4000).

### 7.5.3 SNR comparison of sdLC and tdLC

In order to compare the sensitivity of the current sdLC system to the tdLC system, we measured the SNR of the two detection methods, using a mirror in the sample arm. The optical powers in the sample and reference arm were equal and the acquisition settings in Table 7.1 were applied. For both sdLC and tdLC, the spectrally resolved SNR was determined from the measured spectrum \( S \) using:

\[
\text{SNR} = 10 \cdot \log \left( \frac{SSNR}{\text{var}(\text{noise})} \right) \tag{7.12}
\]

and normalized to zero SNR. In Eq. 7.12 \( \text{var}(\text{noise}) \) denotes the variance of the noise floor in \( S \) for both methods, determined in the wavelength region between 310 and 385 nm where no signal was expected.

Based on Eq. 7.10, we can calculate the expected difference in SNR between both systems. The LCS spectrum covers approximately \( N_s = 1150 \text{ pixels on the USB4000} \). Based on a maximum number of \( 4.10^5 \) counts per photon and a pixel well depth of \( 1.10^5 \) electrons, the quantum efficiency (QE = \#electrons/photon) of the USB4000 is 2.5% at 600 nm. Using the photodiode response of 0.43 A/W (2001, New Focus, USA), we can
calculate that our tdLCS detector has a QE of 89% at 600 nm. With τ=6 ms for our sdLCS system, the sensitivity advantage of the sdLCS measurements described in this Chapter reduces to 0.38. Hence, when using the USB4000 as a detector for sdLCS and the settings in Table 7.1, we can expect a decrease in SNR of 4.2 dB at 600 nm with respect to tdLCS.

![Figure 7.4 Comparison of an sdLCS measurement to a tdLCS measurement of μt, μa and μs on a polystyrene-dye phantom.](image)

Figure 7.4 Comparison of an sdLCS measurement to a tdLCS measurement of μt, μa and μs on a polystyrene-dye phantom.

![Figure 7.5 Signal to noise ratio (SNR) in sdLCS and tdLCS. The investigated spectral range for the measurements in this Chapter runs from 480 to 700 nm (dashed lines).](image)

Figure 7.5 Signal to noise ratio (SNR) in sdLCS and tdLCS. The investigated spectral range for the measurements in this Chapter runs from 480 to 700 nm (dashed lines).

### 7.6 Experimental validation – Results

Figure 7.4 shows the measured μt spectra by sdLCS and tdLCS on the polystyrene-dye phantom. The μt spectra from both detection methods agree within the estimated uncertainties (error bars) for nearly all wavelengths. Also the fits on μt and the μs contributions to the fits agree well, and the μc-contributions are in good agreement
with the Mie calculated $\mu_s$. The fitted dye concentrations were $10.1 \pm 0.4\%$ for the sdLCS measurement and $9.5 \pm 0.4\%$ for the tdLCS measurement, which are both very close to the expected dye concentration of 10%.

Figure 7.5 shows the measured SNR on a mirror. For both sdLCS and tdLCS, the SNR is maximal within the investigated spectral range of 480 to 700 nm. For the majority of wavelengths within this region, the SNR of tdLCS is larger than the SNR of sdLCS, except for the shortest wavelengths ($\lambda < 530$ nm). The decrease in SNR for sdLCS is close to the predicted value of $-4.2$ dB (Section 7.5.3). Note that the SNR value for tdLCS differs from the value given in Chapter 4 (112 dB) due to a difference in method of analysis.

Whereas the SNR in Chapter 4 describes the minimally detectable signal with maximal amplification by the lock-in amplifier, the SNR in this Chapter is obtained with detection settings closer to actual measurements (e.g. with a backscatter coefficient larger than the minimal detectable reflectivity). However, the quantitative value of the SNR is of less importance here, since we primarily consider the differences in SNR in Figure 7.5 for the comparison between sdLCS and tdLCS.

![Figure 7.6 Simulation of the recovered spectrum $S$ for two integration times: $\tau = 0.06$ ms (with $v_R = 60 \mu m/s$) and $\tau = 6$ ms (with $v_R = 6 \mu m/s$).](image)

7.7 Discussion and conclusion

In this Chapter, we demonstrated and validated a new detection method and analysis algorithm for spectroscopic detection in LCS. We showed that this method can be used for measuring local $\mu_r$, $\mu_a$ and $\mu_s$ spectra in turbid media. The results of the sdLCS phantom measurement agreed well with the expected optical properties of the phantom and were comparable to the measured optical properties by tdLCS (Figure 7.4).

The reason to validate this new detection method, is its theoretical sensitivity advantage compared to time domain detection (Section 7.2.2). As a consequence, the acquisition speed of the measurement can be reduced with respect to time domain detection, without reducing the signal to noise ratio. The sdLCS system that was
validated in this Chapter was more than three times faster than the tdLCS system, but not more sensitive (Figure 7.5). A sensitivity advantage for sdLCS could not be demonstrated, because the quantum efficiency of the USB4000 is not optimized for these experiments. However, if the quantum efficiency would be similar to that of our tdLCS detector, the sensitivity advantage would be $10\log(\phi_{3LCS}) = 11$ dB at equal acquisition times for tdLCS and sdLCS (Section 7.5.3).

Figure 7.5 shows a decrease in SNR of approximately 5 dB for sdLCS compared to tdLCS, which is slightly lower than the predicted decrease of 4.2 dB (Section 7.5.3) for these detection settings. The additional decrease in sensitivity can be explained by the relatively slow acquisition speed (167 Hz) of the USB4000. Slow acquisition speeds result in a decrease of the modulation depth in $i_0(\lambda)$ (‘fringe wash-out’), due to the reference mirror movement induced change of $\Delta L$ within the integration time. Hence, the sensitivity of our sdLCS measurements can be improved by increasing the integration time with respect to the velocity of the reference mirror. The effect of fringe wash-out on spectral amplitude has been illustrated in Figure 7.6. Comparable to the simulation in Section 7.3, Figure 7.6 shows the recovered spectra $S$ from a simulation without absorption using integration times of $\tau = 6$ ms and $\tau = 0.06$ ms and reference mirror velocities of 6 $\mu$m/s and 60 $\mu$m/s, respectively. Note that the integration times differ two orders of magnitude, whereas the reference mirror velocities only differ one order of magnitude. As a consequence, the spectrum $S$ for $\tau = 0.06$ ms has a higher amplitude ($\pm15\%$, corresponding to 0.6 dB) and shows better agreement with the input sample arm spectrum ($S_0$) than the spectrum $S$ for $\tau = 6$ ms. This simulation shows that, besides improvements on quantum efficiency, a faster spectrograph will further improve the performance of our sdLCS system. Since high quantum efficiency line scan cameras are available with line rates up to 140 kHz (e.g. the Basler Sprint spL4096-140km, Basler AG, Germany), enhanced sensitivity and/or acquisition speed are realizable for sdLCS.

The only technique that is reported to have comparable performance to our sdLCS system in terms of localized measurements of optical properties, is dual band sOCT [6,7]. However, this method may not be as well applicable on thin layers or small tissue volumes as our LCS system [3], since the spatial dimensions of the largest of the dual bands in this method may extend the dimensions of the volume of interest. In addition, our sdLCS system has the unique advantage of focus tracking, which prevents unwanted signal attenuation and a decrease in sensitivity at larger path lengths in the medium. This facilitates the exact determination of $\mu_s$ and $\mu_t$ contributions to the measured $\mu_t$.

In conclusion, the new approach for sdLCS demonstrated in this Chapter has high potential to improve the accuracy and speed of localized optical property measurements by LCS. Undoubtedly, this will lead to improved clinical utility of the technique, e.g. for the non-invasive determination of blood composition (hemoglobin/bilirubin concentration and oxygen saturation).

References


12. Data tabulated from various sources compiled by S. Prahl, http://omlc.ogi.edu/spectra