Clinical and molecular classification of very early arthritis patients
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CHARACTERISTICS OF SYNOVIAL INFLAMMATION IN EARLY ARTHRITIS ANALYZED BY PIXEL-BY PIXEL TIME-INTENSITY CURVE SHAPE ANALYSIS

M.G.H. van de Sande, C. van der Leij, C. Lavini, C.A. Wijbrandts, M. Maas, P.P. Tak
ABSTRACT

Objectives: Dynamic contrast-enhanced (DCE) magnetic resonance imaging (MRI) time-intensity curve (TIC) shape analysis has previously been used in oncology, where fast initial enhancement and early washout are associated with malignancy. As rheumatoid arthritis (RA) synovium has some ‘tumor-like’ features, we investigated DCE-MRI TIC shape expression in early arthritis in relationship to diagnosis.

Methods: Twenty-eight disease-modifying antirheumatic drug (DMARD) naïve, early arthritis patients (<1 year) with inflammation of at least one knee joint were included. At baseline DCE-MRI of the inflamed knee joint was performed, and TIC shape type expression, maximal enhancement, maximum slope of increase and total volume of enhancing pixels were calculated. In addition, disease activity parameters were determined. At 2 years follow-up, patients were classified as RA or non-RA according to established classification criteria.

Results: Type 4 TIC shape, characterized by fast initial enhancement followed by a quick washout phase, was significantly higher in patients fulfilling classification criteria for RA after 2 years follow-up compared with non-RA patients (15.6% and 7.9%, respectively, \( P = 0.02 \)). All other DCE-MRI parameters showed no differences between the groups, highlighting the specificity of this observation.

Conclusions: A high expression of “aggressive” DCE-MRI TIC shape type 4 is associated with RA. Our results are consistent with the view that increased vascularity plays a key role in the pathogenesis of RA. This study underlines the rationale for further studies investigating the prospect of DCE-MRI TIC shape analysis as a diagnostic tool in early arthritis and the relationship with development of destructive disease.
INTRODUCTION

The synovium is the main affected tissue in inflammatory joint diseases: inflamed synovial tissue is characterized by hypertrophy, influx of inflammatory cells, and neovascularization. Contrast-enhanced magnetic resonance imaging (MRI) is considered the gold standard for imaging synovitis;[1,2] the contrast agent increases the synovial conspicuity and allows for visualization and volume measurements.

In dynamic contrast-enhanced (DCE)-MRI the uptake of contrast agent in time is visualized in a time-intensity curve (TIC). The shape of this TIC is determined by tissue characteristics, such as vascularization, tissue perfusion, capillary permeability and interstitial space volume, which are influenced by the degree of inflammation.[3] Computer-assisted analysis of the TIC provides quantitative assessment of synovitis. Previous studies have applied pharmacokinetic modelling and descriptive parameters, such as maximum enhancement (ME) and maximum slope of increase (MSI) to quantify synovial inflammation.[4] The TIC shape with fast initial enhancement and early washout is associated with malignant tumors.[5,6] Since neovascularization, increased capillary permeability and invasive growth into surrounding tissues can be seen in both malignant tumors and RA, it is conceivable that this specific TIC shape might also be associated with RA.

Recently, we have developed a new technique in which TIC shape expression can be analyzed pixel-by-pixel in a three-dimensional (3-D) volume.[7] This analysis technique is less computationally demanding and at the same time more robust, as it does not make use of model assumptions or non-linear fitting compared with descriptive and pharmacokinetic analysis. In a pilot study [8] we have shown that type 4 TIC shape expression, characterized by fast initial enhancement followed by early washout, appears to be increased in RA patients compared with healthy controls, thereby discriminating between inflamed and non-inflamed joints.

Based on the observations in malignant tumors and the changes in vascularity in patients with arthritis, we wanted to compare the DCE-MRI parameters in RA compared to other inflammatory joint diseases in a pilot study.

PATIENTS AND METHODS

Study patients

Twenty-eight patients with arthritis of at least one knee joint, who had been included in our early arthritis cohort between February 2003 and April 2006, were consecutively enrolled in the current study. All patients had arthritis duration of less than 12 months and were disease modifying anti-rheumatic drug (DMARD) naïve. Patients were excluded if there were contraindications for (contrast-enhanced) MRI, such as claustrophobia, metal implants or elevated serum creatinine.

This study was approved by the Institutional Review Board of the Academic Medical Center and performed in accordance with the Declaration of Helsinki. All study participants gave written informed consent.
Study design
At inclusion DCE-MRI of the inflamed knee joint (if both knees were inflamed the most inflamed joint was evaluated) was performed and demographics and disease activity parameters were determined (as described below). The presence of IgM rheumatoid factor (IgM-RF) and anti-citrullinated protein antibodies (ACPA) was measured by IgM-RF ELISA (Sanquin, Amsterdam, the Netherlands) and anti-CCP2 ELISA (Euro-Diagnostica, Arnhem, the Netherlands), respectively. At a 2-year follow-up visit, patients were classified as either RA or non-RA according to 1987 ACR RA classification criteria [9].

Disease activity parameters
We assessed overall disease activity by the 68 tender and 66 swollen joint score, morning stiffness, patient’s visual analog scale (VAS) of global disease activity (scale 0-100 mm), erythrocyte sedimentation rate (ESR) and C-reactive protein (CRP) levels. Local disease activity of the scanned knee joint was assessed by a patient’s VAS of local disease activity and pain (scale 0-100 mm). Knee joint pain and swelling were also rated by a medical examiner on a semiquantitative scale from 0-3.

MRI data acquisition
MRI of the affected knee joint was performed on a 1.5 T MR-scanner (GE Signa Horizon Echospeed LX9.0, General Electric Medical Systems, Milwaukee, WI) using a 3-D, T1-weighted gradient echo dynamic sequence that consisted of 20 consecutive acquisitions of 20 slices with a temporal resolution of 22 seconds (TR/TE/flip 8.1ms/3.5ms/30, slice thickness 4 mm, FOV 18 cm, 256*256 matrix, axial orientation). The total imaging time of the DCE-MRI acquisition was 7 minutes and 19 seconds.

Patients were placed supine with the knee joint centrally in the magnetic field in a dedicated extremity coil (quadrature detection). A 20 gauge needle infusion line was inserted, preferably in the right antecubital vein. Sixty seconds after the initiation of the dynamic protocol, a bolus of a Gd-DTPA contrast agent (Magnevist, Schering AG, Berlin, Germany; 0.1 mmol/kg) followed by a 15 mL saline chase was delivered at an injection rate of 5 mL/s using an automatic injection device (Spectris MR Injector, MEDRAD, Warrendale, PA).

DCE-MRI analysis
Images were processed using an in-house developed program [10] based on Matlab software (The Mathworks, Natick, MA). This program analyzes the time-dependent signal intensity changes of every voxel (volumetric pixel) in an imaged volume resulting in a time-intensity curve (TIC). Each TIC of every voxel is classified into one of seven predefined TIC shape categories. Every TIC shape type is associated with a color. TIC shape distribution of each image section is visualized in color coded maps [7,8] (see also Figure 2) or when analyzing contiguous sections in three-dimensional parametric TIC shape volumes.[8]

All analyses were performed in a 3-D volume, covering the entire synovial lining of the knee joint from the tibia plateau up to the twelfth proximal slice (approximately 5 cm). Region of interest (ROI) was manually drawn in each slice to exclude enhancing skin and muscle tissue. The nonenhancing tissue (e.g., bone and cartilage) within the ROIs is ignored by the analysis software, which leaves the enhancing synovial tissue and vascular structures within the ROI for analysis.
The total number of enhancing pixels was calculated and percentage of voxels expressing each TIC shape type were calculated (% = number of voxels of a specific TIC shape divided by total number of enhancing voxels within the entire synovial volume). This was done to correct for differences in knee joint size between the patients. In our analysis we only compared expression of TIC shape type 2-5, as these types represent enhancing synovial tissue in the ROI. TIC shape type 6 representing vessels and type 7 representing undefined pixels (which is seen in very low number of pixels [median 0.3%]) were used only for the calculation of the percentage per TIC shape type.[8]

In a similar way, the image analysis program calculated the maximal enhancement (defined as the difference between maximal signal intensity and baseline, divided by signal baseline), time to peak (defined as the time between the start of enhancement and maximal signal intensity), and maximum slope of increase (defined as the largest positive signal difference between two successive acquisitions) for each voxel in the imaged volume and calculated the average values.[8]

**Statistical analysis**

Standard statistical software (SPSS version 16, SPSS, Chicago, IL) was used for statistical analysis. Chi-square test (for categorical data) or Mann-Whitney U test (for numerical data) was used to determine significant differences between both patient groups. Correlations between clinical parameters and DCE-MRI parameters were assessed with the Spearman rank-order correlation coefficient. Values were expressed as percentages (female), number of positive patients (IgM RF and ACPA) or median and interquartile range (IQR). Statistical significance was defined as \( P < 0.05 \). As we wanted to explore parameters with a potential to be used as a discriminative marker, we did not correct for multiple testing.

**RESULTS**

**Disease activity and RA diagnosis**

No patients were excluded based on contra-indications for MRI. Of the 28 included patients, 7 patients were classified as RA and 21 patients as non-RA at 2 years of follow-up. The non-RA group consisted of patients with spondylarthritis (\( n=2 \)), crystal arthropathy (\( n=1 \)), HIV-related arthritis (\( n=1 \)), and undifferentiated arthritis (\( n=17 \)). Demographics and clinical characteristics are summarized in Table 1.

A significantly higher number (median (IQR)) of tender (16 (14) versus 2 (5), \( P < 0.001 \)) and swollen (8 (17) versus 2 (4), \( P=0.01 \)) joint counts, increased CRP levels (15.0 (47.0) versus 3.0 (5.4) mg/L, \( P=0.02 \)) and percentage of ACPA positive patients (\( P=0.02 \)) were observed in the RA compared with the non-RA patient group. Otherwise, there were no statistically significant differences between the groups.

**A high percentage of type 4 TIC shape is associated with RA**

We observed a significantly higher percentage of type 4 TIC shape (fast initial enhancement followed by a quick washout phase) in the RA patient group compared with the non-RA group (15.6% (6.6) and 7.9% (7.6), respectively, \( P=0.02 \)) (Figure 1). Figure 2 shows examples of TIC expression in an RA patient and in a non-RA patient. Percentages of enhancement of the other
Table 1. Baseline patient characteristics.

<table>
<thead>
<tr>
<th></th>
<th>All (n=28)</th>
<th>RA (n=7)</th>
<th>Non-RA (n=21)</th>
<th>P-value</th>
</tr>
</thead>
<tbody>
<tr>
<td>Female (n)</td>
<td>17</td>
<td>5</td>
<td>12</td>
<td>0.56*</td>
</tr>
<tr>
<td>Age (years)</td>
<td>47 (22)</td>
<td>48 (32)</td>
<td>48 (19)</td>
<td>0.69*</td>
</tr>
<tr>
<td>68 Tender joint count (n)</td>
<td>3 (11)</td>
<td>16 (14)</td>
<td>2 (5)</td>
<td>&lt;0.001*</td>
</tr>
<tr>
<td>66 Swollen joint count (n)</td>
<td>2.5 (4)</td>
<td>8 (17)</td>
<td>2 (4)</td>
<td>0.01*</td>
</tr>
<tr>
<td>Patient’s global VAS (0-100 mm)</td>
<td>51 (39)</td>
<td>52 (40)</td>
<td>49 (40)</td>
<td>0.83*</td>
</tr>
<tr>
<td>Morning stiffness (min)</td>
<td>25 (57)</td>
<td>60 (30)</td>
<td>20 (52)</td>
<td>0.11*</td>
</tr>
<tr>
<td>CRP (mg/L)</td>
<td>4.8 (15.0)</td>
<td>15.0 (47.0)</td>
<td>3.0 (5.4)</td>
<td>0.02*</td>
</tr>
<tr>
<td>ESR (mm/hr)</td>
<td>16 (34)</td>
<td>33 (39)</td>
<td>14 (34)</td>
<td>0.12*</td>
</tr>
<tr>
<td>Patient’s local disease activity VAS (0-100 mm)</td>
<td>42 (55)</td>
<td>81 (60)</td>
<td>35 (38)</td>
<td>0.08*</td>
</tr>
<tr>
<td>Patient’s local pain VAS (0-100 mm)</td>
<td>37 (33)</td>
<td>33 (72)</td>
<td>37 (49)</td>
<td>0.78*</td>
</tr>
<tr>
<td>Examiner’s local swelling (0-3)</td>
<td>1 (1)</td>
<td>1 (1)</td>
<td>1 (1)</td>
<td>0.81*</td>
</tr>
<tr>
<td>Examiner’s local pain (0-3)</td>
<td>1 (1)</td>
<td>1 (1)</td>
<td>1 (1)</td>
<td>0.12*</td>
</tr>
<tr>
<td>IgM rheumatoid factor positive (n)</td>
<td>4</td>
<td>2</td>
<td>2</td>
<td>0.21*</td>
</tr>
<tr>
<td>ACPA positive (n)</td>
<td>7</td>
<td>4</td>
<td>3</td>
<td>0.02†</td>
</tr>
</tbody>
</table>

Medians (IQR) or number of patients are shown. Mann Whitney U test (*) or Chi-square test (†), was used to compare both groups. P-values < 0.05 were considered to be statistically significant. VAS = visual analog scale, CRP = C-reactive protein, ESR = erythrocyte sedimentation rate, ACPA = anti-citrullinated protein antibodies.

three TIC shape types, ME, initial rate of enhancement and total number of enhancing pixels (representing the total volume of inflamed synovial tissue) did not show statistical differences between the two groups (Table 2). No significant correlations were observed between the different disease activity parameters and type 4 TIC shape expression in the whole patient group (data not shown).

**DISCUSSION**

In this study we evaluated the DCE-MRI TICs in early arthritis patients. A significantly higher percentage of type 4 TIC shape expression in RA patients compared with non-RA patients was seen, but there were no differences in the DCE-MRI descriptive parameters ME and initial rate of enhancement. This latter observation is in line with previous studies comparing RA with disease controls using descriptive DCE-MRI parameters that were similar for RA and controls. [11] Therefore, in contrast to the generally used, descriptive-only DCE-MRI analysis, the present study suggests that TIC shape analysis might have value in differentiating between RA and non-RA using DCE-MRI. However, as there was a fair overlap between the RA and non-RA patient group, the discriminative value of the type 4 TIC needs to be studied in a larger cohort to evaluate if this analysis has additional value over standard diagnostic parameters.
Figure 1. Expression of Time Intensity Curve (TIC) type expression in non-RA (0) and RA (1) patients. TIC type is expressed as percentage of total enhanced voxels.

Figure 2. Time-intensity curve shape maps (1 image slice) of the knee joint of an RA patient (A) and a non-RA patient (B). The maps show marked enhancement of the synovial tissue with mainly type 3 and 4 TIC-shapes in the RA patient and mainly type 2 and 3 TIC shapes in the non-RA patient. Types of time intensity curve (TIC) shapes shown on the right side. Type 1: no enhancement, type 2: gradual increase of enhancement, type 3, 4, and 5: fast initial enhancement followed by, resp. a plateau phase, an early washout phase, sustained late enhancement, type 6: arterial enhancement, type 7: all others.

In previous studies examining synovitis, DCE descriptive parameters were either calculated from a single slice or by averaging multiple slices (reviewed in [4]). This might have resulted in an over- or underestimation of the level of inflammation, as inflammation is known to be heterogeneously distributed throughout the synovial tissue. In our study we evaluated the pixel-by-pixel expression of different TIC shape types in whole synovial volume (without averaging values of separate slices), respecting the heterogeneity of inflammation within the
tissue. This may be one of the reasons that TIC shape analysis enabled us to observe differences between the RA and non-RA patients, while total enhanced synovial volume was comparable between both groups.

Besides DCE-MRI, the value of static contrast-enhanced MRI parameters, such as synovial volume and bone edema, have been studied in relationship to diagnosis and outcome. The diagnostic value of MRI parameters has been variable between various studies.[12] Although some studies have shown a clear association between presence of bone edema and development of erosions [13-15] because of the low predictive value of these parameters it has been recommended not to use MRI in regular clinical care.[12]

We used in house developed software to perform the analysis.[10] This software can in principle be applied in other centers. Recently other groups have started developing similar sort of analysis software,[16] and we expect these will be soon available commercially.

The type 4 TIC shape is mostly seen in more aggressive tumor types and helps to differentiate benign from malignant tumors.[6,17] Consistent with these findings, type 4 TIC shape was relatively more present in RA, a disease characterized by autonomous disease progression [18] and, if not adequately treated, destructive disease. Physiological tissue features, such as vascularization, vessel perfusion, vessel permeability and interstitial space volume, determine the shape of the TIC.[3,19] Neovascularization and influx of inflammatory cells seen during inflammation can influence these tissue features, and thereby the TIC shape. Types 3, 4, and 5 TIC are all characterized by fast initial enhancement, whereas only in TIC type 4 this fast enhancement is followed by a quick washout phase. Vessel permeability and interstitial space volume are both known to be of significance during this washout phase [20] and could determine the difference between RA and non-RA patients. Type 4 TIC shape is associated with invasive growth in tumors. Conceivably, in RA TIC type 4 expression might be related to the invasive growth, leading to the development of joint destruction. Specifically, studying TIC type 4 expression in the synovium at sites prone to development of erosions might be of interest. Because of the relative low number of RA patients investigated, this is beyond the scope of the present study.

In the group of non-RA patients, three patients had ACPA-positive UA. In these patients low numbers of TIC shape type 4 expression were observed. Possibly, these patients are ACPA positive arthritis patients with a relatively mild form of arthritis who do not progress to RA when treated in an early phase. In our previous study in pre-clinical arthritis patients we have shown that ACPA positive pre-clinical RA patients do not have an increased expression of TIC type 4 similar to healthy individuals.[8] It might be that there is a spectrum of ACPA positive synovitis that can develop into self-limiting arthritis and into full-blown RA.

A limitation of this study is the relatively small number of patients, especially in the RA subgroup. However, a statistically significant difference in type 4 TIC shape was still observed, which could not be explained by outliers. This study provides the rationale for larger studies in the future to determine the exact role of pixel-by-pixel TIC shape analysis for differential diagnosis in early RA.

Taken together, this is the first description of DCE-MRI TIC shape analysis in early arthritis patients. Based on the association of a relatively high type 4 TIC shape expression with RA, TIC shape analysis might be useful to differentiate between RA and non-RA patients at an early stage. Furthermore, it provides a rationale to study the relationship between TIC shape expression and development of joint destruction in a larger early RA cohort.
Rheumatology key messages

» The expression of “aggressive” DCE-MRI TIC shape type 4 is increased in early RA

» The presence of DCE-MRI shape type 4 TIC might have potential as a diagnostic biomarker

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