Continuous glucose and exhaled breath analysis in the Intensive Care Unit
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Chapter 4

Intravenous Microdialysis–based Glucose–monitoring Device in Critically Ill Patients – a Prospective Study

Point and Trend Accuracy of a Continuous Intravenous Microdialysis–based Glucose–monitoring Device in Critically Ill Patients – a Prospective Study


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ABSTRACT

Introduction: Microdialysis is a well-established technology that can be used for continuous blood glucose monitoring. We determined point and trend accuracy, and reliability of a microdialysis-based continuous blood glucose-monitoring (CGM) device (EIRUS®) in critically ill patients.

Methods: Prospective study involving patients with an expected intensive care unit (ICU) stay of ≥ 48 hours. Every 15 minutes, device readings were compared with blood glucose values measured in arterial blood during blocks of 8 hours per day for a maximum of three days. The Clarke Error grid, Bland–Altman plot, mean absolute relative difference and glucose prediction error analysis were used to express point accuracy, and the Rate Error Grid to express trend accuracy. Reliability testing included aspects of the device and the external sensor, and the special central venous catheter (CVC) with a semipermeable membrane for use with this device.

Results: We collected 594 paired values in 12 patients (65 [26–80; 8 – 97] [median [IQR; total range]) paired values per patient). Point accuracy: 93.6% of paired values were in zone A of the Clarke error grid, 6.4% were in zones B; bias was 4.1 mg/dL with an upper limit of agreement of 28.6 mg/dL and a lower level of agreement of −20.5 mg/dL in the Bland Altman analysis; 93.6% of the values ≥ 75 mg/dL were within 20% of the reference values in the glucose prediction error analysis; the mean absolute relative difference was 7.5%. Trend accuracy: 96.4% of the paired values were in zone A, and 3.3% and 0.3% were in zones B and zones C of the rate error grid. Reliability: out of 16 sensors, 4 had to be replaced prematurely; out of 12 CVCs, two malfunctioned (one after unintentional flushing by unsupervised nurses of the ports connected to the internal microdialysis chamber, causing rupture of the semipermeable membrane; one for an unknown reason). Device start–up time was 58 [56–67] minutes; availability of real–time data was 100% of the connection time.

Conclusions: In this study in critically ill patients who had no hypoglycemic episodes and a limited number of hyperglycemic excursions, point accuracy of the device was moderate to good. Trend accuracy was very good. The device had no downtimes, but 4 out of 16 external sensors and 2 out of 12 CVCs had practical problems.

INTRODUCTION

Most, if not all critically ill patients receive intravenous infusion of insulin for blood glucose control at some point during stay in the intensive care unit (ICU) [1]. This strategy requires frequent blood glucose measurements for the guidance of insulin titrations, but this is both time and blood-consuming [2]. Automation of blood sampling and glucose measurement through continuous glucose monitor (CGM) devices could reduce this burden, and has the potential...
to improve overall blood glucose control [3,4]. Microdialysis offers the opportunity to sample blood analytes with high accuracy but without the need for drawing blood samples. EIRUS® (Maquet Critical Care AB, Solna, Sweden), a microdialysis–based device that can measure blood glucose and lactate levels, has been tested and validated previously in studies in surgical patients, where it has been found to be safe and accurate [4-7]. To date, its accuracy with regard to blood glucose monitoring, and reliability have not yet been tested extensively in ICU patients [4,6]. We hypothesized the EIRUS® system to be point and trend accurate, and to be reliable in ICU patients. To test this hypothesis, we used this CGM device in a series of critically ill patients, to compare device readings with frequently measured arterial blood glucose values. Along the study, we determined reliability of the device and the special central venous catheter (CVC) with a semi-permeable membrane designed for use with this device.

**METHODS**

**Study design and population**

This investigator–initiated prospective study was conducted in the mixed medical–surgical ICU of the Academic Medical Center, Amsterdam, The Netherlands. The Institutional Review Board of the Academic Medical Center approved the study protocol, and informed consent was obtained from all patients or their legal representatives before start of the study. Maquet Critical Care AB provided the CGM device and its disposables free of charge. Maquet Critical Care AB had neither influence on the design of this study, nor on reporting of the results. The study was registered at the Netherlands Trial Register (NTR4527). Patients were eligible for participation if they were at least 18 years old, were expected to stay in the ICU for ≥ 48 hours, had an arterial catheter in place and were in need of a (new) CVC. Patients were excluded if they participated in another investigational drug or device study, or were known to be pregnant.

**Blood glucose control**

ICU nurses followed a local guideline aiming at a blood glucose level between 90–144 mg/dL (5–8 mmol/L) as part of standard care. This guideline mandated nurses to measure blood glucose every four hours, or more frequently when glucose levels were out of range or when rapid changes were expected. Infusion of insulin was started when glucose levels were over 144 mg/dL and stopped when glucose was lower than 61 mg/dL. Adjustments of insulin titration were based on sliding scales. More details can be found in the online supplement. In addition, details on how nurses were trained can also be found in the online supplement. During the study, ICU nurses were not allowed to change insulin infusion rate.
based on the readings by the device. The ICU nurses, however, had access to device readings and additional arterial blood glucose measurements were allowed if the device suggested rapid changes in the glucose level, or when there was a trend towards hypoglycemia. In addition, the ICU nurses could also adjust insulin infusion rates based on reference blood glucose values obtained during study observation periods (see below).

The study device
For intravenous microdialysis–based glucose monitoring a special CVC with a semi–permeable membrane (Maquet Critical Care AB, Solna, Sweden) is needed. This CVC has five lumens, three ‘normal’ ports for intravenous administration of fluids or medication, and two ‘special’ ports for transport of normal saline alongside the semi–permeable membrane, which should not be flushed and cannot be used for intravenous administration of fluids or medication. The ‘afferent’ port is connected to a saline–filled syringe placed in the syringe pump of the device. The ‘efferent’ port is connected to the disposable sensor. Small metabolites such as glucose pass through the semi–permeable membrane creating equilibrium between blood and the dialysate. The dialysate is pumped over the sensor in a continuous fashion, where the glucose oxidase method is used to measure the glucose level [4,5]. The device can be used for a maximum of 96 hours per sensor. Reference measurements are needed for calibration of the device, which is performed at start–up and every 8 hours thereafter.

Of note, because the dialysate needs to be transported to the sensor outside the patient, where measurements are performed, there is a delay in time of 5 minutes between dialysate formation and the actual measurements.

Study procedures
In three blocks of eight hours per day, and for a maximum of three days, every 15 minutes an arterial blood sample of 200 µl was drawn through an existing arterial line. Blood glucose levels were measured using a blood gas analyzer (RAPIDLab 1265, Siemens Healthcare Diagnostics, The Hague, The Netherlands). Definitions of the metrics used to assess device reliability, including those suggested by recent consensus recommendations [8], are described in detail in the online supplement, and included the percentage of real–time data, skips in data acquisition, failures to calibrate, sensor failures and CVC failures.

Power calculation
Based on previous studies [9,10] we chose to collect approximately 1,000 paired measurements or to connect the device to a minimum number of 11 patients. Inclusion of patients was restricted by the time the device was available for
this study, and the number of disposable CVCs and sensors provided by the manufacturer.

**Analysis plan**

Patient characteristics were reported as means, medians or percentages, where appropriate. Because of the delay between dialysate formation and the actual measurements of the blood glucose level, we subtracted 5 minutes from the timestamp of the values of the CGM device; as such reference blood glucose values matched with the moment dialysate was formed. Subsequently, device and reference measurements were merged. Paired measurements were used for determining point and trend accuracy of the device. To be considered for the statistical analysis, each patient needed to have at least multiple samples with at most 30 minutes in between. However, patients excluded for statistical analysis remained included in the reliability analysis. While each paired sample was included in the point accuracy analysis, only the samples with a gap of at most 30 minutes to the next sample were included in the trend accuracy analysis. In addition, when the device was calibrated within the daily 8–hour block of intense sampling, the calibration sample and the subsequent sample were not considered for trend accuracy analysis. This way, large changes in trend due to the calibration were excluded from the analysis.

Point accuracy was expressed using a Clarke error grid, a Bland–Altman plot, the glucose prediction error analysis, and the mean absolute relative difference (MARD). To be considered point accurate, at least 95% of values must be in zones A, a maximum of 5% can be in zones B, and no values are allowed in zones C to E of the Clarke error grid [11]. Also, the MARD should be below 14%; a value above 18% represent poor accuracy [3].

Trend accuracy was expressed using rate error grid Analysis (R–EGA) [12]. Values outside zones A and B of the R-EGA corresponding to values in zones A and B of the Clarke error grid were considered benign errors. On the other hand, values outside zones A and B of the R-EGA corresponding to values outside zones A and B of the Clarke error grid were considered erroneous readings [12].

**Post–hoc analysis**

Point accuracy was also expressed using the recently published surveillance error grid [13]. Two of the CVCs were malfunctioning. In one case it was immediately clear that the CVC was defect, and no additional measurements were performed. In another case this was not immediately clear, and only after reviewing the readings it became clear that the CVC started to malfunction from a certain timepoint. We chose to perform a post–hoc analysis excluding the data from that patient.
RESULTS
A total of 12 patients were included in whom 598 paired measurements were available. Figure 1 shows the CONSORT diagram. One patient was excluded from the point and trend accuracy analyses because no comparative samples could be obtained while the device was connected due to calibration problems. In one patient, four arterial blood samples had to be discarded as they were diluted during sampling. Thus we had 594 samples (65 [26 – 80; 8 – 97] (median [IQR; total range]) paired values per patient) for determining point accuracy of the CGM device. For trend accuracy analysis, 482 samples were used. Patient characteristics are shown in Table 1. Metrics of glucose control are shown in Table 2.

Point and trend accuracy
The Clarke error grid, Bland–Altman plot, and glucose prediction error grid are presented in Figure 2. Bias in the Bland–Altman plot was 4.1 mg/dL with an upper limit of agreement of 28.6 mg/dL and a lower limit of agreement of -20.5 mg/dL. Glucose prediction error analysis showed that 93.6% of the values ≥ 75 mg/dL within twenty percent of the values measured by the blood gas analyzer were within range. The MARD was 7.5%. The rate error grid is presented in Figure 3, consisting of 99.7% accurate readings and 0.3% benign errors.

Reliability
Table 3 shows reliability results. Start–up time was 58 [56 – 67; 48 – 112.8] (median [IQR; total range]) minutes. In three patients, the initial sensor could not be calibrated at start–up, and a second sensor was needed. In two patients, the CVC malfunctioned after some hours. In one patient, this was due to improper handling by one of the trained ICU nurses. This and other details on reliability are discussed in more detail in the online supplement.

Post–hoc analysis.
The Surveillance error grid is presented in Figure S1 in the supplement. Results of the post–hoc analysis excluding the data from the patient mentioned above in whom the CVC was malfunctioning for unknown reasons is presented in online supplement Figures S3, S4 and S5.

DISCUSSION
In this study in a cohort of critically ill patients, point accuracy of a microdialysis–based CGM device developed was moderate to good. Trend accuracy was very good. Reliability was moderate, seen as 4 out of 16 external sensors could not be used and 2 out of 12 CVCs had practical problems. Point accuracy in the present study was less than the point accuracy reported
from two previous studies in patients after cardiac surgery [4, 6]. In these study, all paired values were in zones A and B, with 97% and 99% of values in zones A of the Clark error grid, and the MARD was only 5.6% and 5%, respectively. Both those studies, and the present study used arterial blood gas analyzers as a reference standard. The present study, however, was conducted in patients that were more severely ill than cardiac surgery patients, reflected by a longer length of stay in the ICU stay (15 vs. 3 days) and hospital (20 vs. 8 days). Thus, these two studies included completely different patients, which could, at least in part explain the differences. The results of the present study, however, are very similar to a pilot study in abdominal surgery patients [5], in which all paired values were in zone A and B, with 94% of values in zones A of the Clark error grid.

According to a recent consensus on blood glucose monitoring, 95% of paired values need to be in zones A of the Clarke error grid to qualify a device as point accurate [11]. In contrast, a more recent consensus amongst a panel of ICU experts, the MARD should be < 14% [3]. While the studied device did not meet the first criteria, it did meet the last. There are no generally accepted criteria for trend accuracy of CGM devices in the ICU setting [3]. Nonetheless, we believe EIRUS to be very accurate, as only one value was in the benign error range[12]. In addition, it should be noted that the paired measurement in zone C mentioned above came from the patient in whom the special CVC was malfunctioning. Since both glucose and lactate measured by the device decreased rapidly and non-physiologically, we suspect that the semipermeable membrane of that CVC broke.

Both the afferent and efferent ports of the CVC, connected to the dialysate chamber, were labeled with tags mentioning not to flush these ports. Unfortunately, unsupervised nurses thought there was backflow of blood in the afferent port because of the deep-red/purple color, and flushed it with normal saline immediately. This resulted in a rupture of the delicate semi-permeable membrane, and thus malfunctioning of the CVC: saline pumped into the chamber disappeared into the circulation, and the efferent port stopped producing dialysate. After this we continued using the special CVC as a normal CVC, with two stops at the extra ports. The manufacturer changed the color of the lumen and its connector to prevent this incident after this study. These problems however, did raise some concerns. However, we do not believe that these problems were caused by an insufficient introduction of the study device in the unit since we organized multiple training sessions for nurses and instructed nurses individually when a patient was included in the study and monitored by the device.

Our study has several limitations. First and most importantly, no hypoglycemic periods were captured during the study, and the number of hyperglycemic
events was small. While the device proved point accurate in the hypoglycemic range in one study in animals [14], we remain uncertain on hypoglycemic performance in ICU patients. The absence of hypoglycemia might be explained by the fact that reference measurements were performed very frequently, and because nurses had access to the device readings. Nurses were allowed to use the reference measurements, and thus could improve blood glucose control (i.e., prevent hypoglycemic events). Even the device readings could have helped nurses to prevent dangerous excursions of the blood glucose level, even though they knew that this was an investigational device. The local Institutional Review Board did not accept blinding the nurses for the reference measurements and the device readings. In addition, the fact that we only actively collected paired measurements during day-time hours means that we might have missed possible interesting data overnight. More paired samples, also outside working hours, could have yielded more hypoglycemic events. To make a more conclusive statement on device accuracy in the hypoglycemic range, other methods for capturing hypoglycemic and hyperglycemic events have to be further explored. One recently suggested way to improve the execution of accuracy testing of investigational devices in the clinical setting includes data mining of electronic medical records [15,16]. Data mining is a technique that uses large quantities of data in search for certain events, in this case hypoglycemia and hyperglycemia. Comparison between consecutive measurements of the blood glucose level by means of a CGM device and comparative measurements in a central laboratory then could be used to determine the accuracy in these extreme situations. This approach certainly increases the number of hypoglycemic and hyperglycemic events that can be used for accuracy testing, but of course requires extensive use in one or more intensive care units. Finally, as of September of 2015, shortly after analyzing the data before reaching our goal of 1,000 paired samples, we had to stop the study prematurely. The data allowed for a sufficiently narrow interval of confidence on the point and trend accuracy of the machine and therefore we did not consider it ethically justified to include more patients, seen the potential burden and risks of obtaining blood samples every 15 minutes.

There were also several strengths to this study. This is the first study to date to investigate trend accuracy of a CGM device in critically ill patients. In addition, the investigated microdialysis CGM device had not been tested in a mixed ICU before. This makes the results of this study more clinically applicable as this is indeed the patient population in which glucose monitoring is most relevant. Finally, we used precise blood gas analyzers for reference measurements, and we corrected for the 5-minute delay between formation of the dialysate and the measurement at the sensor side.
CONCLUSION

The point and trend accuracy of the tested microdialysis-based CGM device was moderate to good in patients who were stable with regard to their blood glucose levels. Trend accuracy was very good. The device had no downtimes, but 4 out of 16 external sensors and 2 out of 12 CVCs had practical problems.

References

FIGURES

Patients screened
N = 2794

Excluded:
- Expected stay < 48 h       N = 1141
- Missed or wrong CVC        N = 688
- No CVC                     N = 618
- No arterial line           N = 317
- Age < 18                   N = 20
- In other trial             N = 4
- No informed consent        N = 3
- Pregnant                   N = 1

Included
N = 12

No paired measurements       N = 1

Included in accuracy analysis
N = 11

Figure 1.
CONSORT diagram.
Figure 2.
Measures of point accuracy. Bland–Altman plot (upper left panel), glucose prediction error grid (lower left panel) and Clarke error grid (right panel).

Continuous Glucose - Error Grid Analysis

Figure 3.
Rate Error–Grid of the Continuous glucose–error grid analysis. This grid is divided into similar zones as the Clarke error grid. Perfectly trend accurate values are the dashed line in the middle.
### Table 1. Patient characteristics

IQR, Interquartile range; BMI, body mass index; APACHE II, Acute Physiology and Chronic Health Evaluation II; SAPS II, Sepsis-related Organ Failure Assessment score II; ICU, Intensive Care Unit; LOS, Length of stay.
Total number of measurements 594
Mean blood glucose level per patient, mg/dL, median [IQR; total range] 133 [118 – 140; 112 – 162]
Standard deviation of blood glucose level per patient, mg/dL, median [IQR; total range] 15 [11 – 18; 1 – 49]
Number of measurements per patient, median, [IQR; total range] 65 [26 – 80; 8 – 97]
Mild hyperglycemia 150-179 mg/dL in measurements, number (%) 62 (10)
Mild hyperglycemia 150-179 mg/dL in patients, number (%) 10 (91)
Severe hyperglycemia >180 mg/dL in measurements, number (%) 29 (5)
Severe hyperglycemia >180 mg/dL in patients, number (%) 3 (27)
Severe hypoglycemia ≤40 mg/dL in measurements, number (%) 0
Severe hypoglycemia ≤40 mg/dL in patients, number (%) 0
Mild hypoglycemia 41-70 mg/dL in measurements, number (%) 0
Mild hypoglycemia 41-70 mg/dL in patients, number (%) 0

Table 2.
Metrics of glucose control. IQR, Interquartile range

<table>
<thead>
<tr>
<th></th>
<th>In total</th>
<th>Per patient</th>
</tr>
</thead>
<tbody>
<tr>
<td>Total number of sensors used</td>
<td>16</td>
<td>1.0 [1.0–2.0; 1 – 2]</td>
</tr>
<tr>
<td>Total connection time, median [IQR; total range]</td>
<td>50.8 [13.5–54.7; 2.5 – 55.8] hours</td>
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<tr>
<td>Real–time data, median [IQR; total range] (%)</td>
<td>50.8 [13.5–54.7; 2.5 – 55.8] hours (100%)</td>
<td></td>
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<tr>
<td>Time of skips in data acquisition</td>
<td>0.0 hours</td>
<td></td>
</tr>
<tr>
<td>Percentage of time skips in data acquisition</td>
<td>0.0 hours</td>
<td></td>
</tr>
<tr>
<td>Initialization time, median [IQR; total range]</td>
<td>42 [42–43; 40.8 – 62.4] minutes</td>
<td></td>
</tr>
<tr>
<td>Total start-up time, median [IQR; total range]</td>
<td>58 [56–67; 48 – 112.8] minutes</td>
<td></td>
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<tr>
<td>Number of calibrations needed before start, median [IQR; total range]</td>
<td>1.0 [1.0–1.3; 1 – 3]</td>
<td></td>
</tr>
<tr>
<td>Number of calibrations during duration of measurement, median [IQR; total range]</td>
<td>6.5 [2.0–7.0; 1 – 8]</td>
<td></td>
</tr>
<tr>
<td>Number of failed calibrations during duration of measurement, median [IQR; total range]</td>
<td>0.5 [0.0–2.0; 0 – 3]</td>
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Table 3.
Reliability and safety of the CGM device
SUPPLEMENTAL INFORMATION

Guideline for glucose control
A local guideline aiming at a blood glucose level between 90–144 mg/dL (5–8 mmol/L) was followed as part of standard care with insulin infusion being initiated when glucose levels rose over 144 mg/dL. When glucose levels were below 61 mg/dL insulin infusion was stopped and boluses of dextrose were given. Sliding scales were used for the adjustment of insulin titration. Insulin was only infused intravenously and in a continuous manner and boluses were exclusively administered when blood glucose levels rose over 360 mg/dL.

The guideline mandated nurses to measure blood glucose at least every four hours, or more frequently when glucose levels were out of range or when rapid changes were expected. Blood gas analyzers (RAPIDLab 1265, Siemens Health-care Diagnostics, The Hague, The Netherlands) were used to analyze the samples. Data was stored in the patient data management system.

Training of the nurses and the use of the device
Before the study device was introduced into the unit, nurses were trained on how to use and calibrate the device. When a patient was eligible for inclusion in the study and after placement of the special CVC was placed the device was connected by the researchers who performed the first calibrations. Nurses were instructed on how to use the CVC, in particular not to flush the two special ports used by the CGM device. In addition, both ports were labeled with adhesive tags clearly showing the following text: ‘DO NOT FLUSH’ (in Dutch: ‘NIET FLUSHEN’).

Metrics for device reliability
- Total number of sensors used – Total number of sensors used between all patients.
- Number of sensors used – Number of sensors used per patient.
- Total connection time – Total connection time the system was connected to a patient.
- Real-time data – Total time the data was displayed in real-time.
- Time of skips in data acquisition – Time the data was not displayed.
- Percentage of time skips in data acquisition – Percentage of the time the data was not displayed.
- Initialization time – Total time from connecting the device, to being ready for calibration.
- Total start-up time - Total time from connecting the device, to displaying the first glucose value.
- Number of calibrations needed before start – Number of calibrations that
were necessary before first glucose value was displayed.

- Number of calibrations during duration of measurement – Total number of calibrations that were performed during the time the device was connected to the patient.
- Number of failed calibrations during duration of measurement – Number of calibrations that failed during the time the device was connected to the patient.

**Reliability and practical problems**
In three patients, the initial sensor could not be calibrated at start-up, and a second sensor was needed. In one patient, the device gave repeated calibration problems, also after replacing the sensor. No measurements could be taken in this patient. This is the aforementioned patient that was excluded from the point and trend accuracy analysis. Calibrated sensors had no down-times and displayed values for 100% of the connection time. In one patient, a non-supervised but trained ICU nurse unintentionally flushed the afferent port of the CVC, causing an abrupt rupture of the semipermeable membrane, and consequently this CVC could no longer be used for continuous blood glucose monitoring (data from this patient were excluded from the point and trend accuracy analysis). In another patient the CVC malfunctioned for an unknown reason. While device data showed a stop in flow, possibly caused by membrane rupture, the nurse denied flushing the special ports of the CVC. Figure S2 shows that the trend in blood glucose levels was comparable to that of blood lactate levels. The non-physiologic drop in lactate allowed us to identify malfunctioning of the CVC, for yet unknown reasons.

**POST-HOC ANALYSIS EXCLUDING DATA FROM ONE PATIENT WITH A MALFUNCTIONING CVC**

**Methods**
To investigate if the special CVC was malfunctioning in this patient, we analyzed both continuous glucose and lactate data as measured by EIRUS® system and plotted the values against reference values from our blood gas analyzer. To investigate the point and trend accuracy of EIRUS® system without the patient in whom the special CVC was malfunctioning, data from the aforementioned patient was excluded. Thereafter, the same instruments were used to analyze point – and trend accuracy. Point accuracy was expressed using a Clarke error grid, a Bland–Altman plot, the glucose prediction error analysis, the mean absolute relative difference (MARD) and the Surveillance error grid. Trend accuracy was expressed using rate error grid Analysis (R–EGA).
Results
As can been seen in figure S2, both glucose and lactate values as measured by the EIRUSTM drop significantly within 15 minutes (133 mg/dL to 90 mg/dL and 23 mg/dL to 17 mg/dL, respectively). We consider this fast change to be implausible. In addition, the monitor intermittently displayed the message that it was flushing the line. Therefore, we suspect that the CVC was not performing correctly, possibly after being flushed.

A total of 582 paired measurements in 10 patients were analyzed. The Clarke error grid, Bland–Altman plot, and glucose prediction error grid of the post-hoc analysis are presented in Figure S3. Bias in the Bland–Altman plot was 4.0 mg/dL with an upper limit of agreement of 28.0 mg/dL and a lower limit of agreement of -19.9 mg/dL. Glucose prediction error analysis showed that 94.3% of the values ≥ 75 mg/dL within twenty percent of the values measured by the blood gas analyzer were within range. The MARD was 7.3%. The rate error grid is presented in Figure S4. The Surveillance error grid is presented in figure S5.
Figure S1
Surveillance error grid with risk scores.
Figure S2.
Blood glucose, CGM and lactate values of patient with failing CVC
Figure S3.
Measures of point accuracy. Bland-Altman plot (upper-left panel), glucose prediction error grid (lower-left panel) and clarke error grid (right panel).

Figure S4.
Rate Error–Grid of the Continuous glucose–error grid analysis This grid is divided into similar zones as the clarke error grid. Perfectly trend accurate values are the dashed line in the middle.
Figure S5.
Post-hoc Surveillance error grid with risk scores.