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Training a Spiking Neural Network with Equilibrium Propagation

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Abstract

Backpropagation is almost universally used to train artificial neural networks. However, there are several reasons that backpropagation could not be plausibly implemented by biological neurons. Among these are the facts that (1) biological neurons appear to lack any mechanism for sending gradients backwards across synapses, and (2) biological “spiking” neurons emit binary signals, whereas back-propagation requires that neurons communicate continuous values between one another. Recently Scellier and Bengio [2017], demonstrated an alternative to backpropagation, called Equilibrium Propagation, wherein gradients are implicitly computed by the dynamics of the neural network, so that neurons do not need an internal mechanism for backpropagation of gradients. This provides an interesting solution to problem (1). In this paper, we address problem (2) by proposing a way in which Equilibrium Propagation can be implemented with neurons which are constrained to just communicate binary values at each time step. We show that with appropriate step-size annealing, we can converge to the same fixed-point as a real-valued neural network, and that with predictive coding, we can make this convergence much faster. We demonstrate that the resulting model can be used to train a spiking neural network using the update scheme from Equilibrium propagation.

1 Introduction

The human brain, a network of around $10^{11}$ neurons, consumes around 20W [Ling, 2001]. For comparison, a Titan X GPU running real-time object detection with YOLO [Redmon et al., 2016], a network of around $10^7$ neurons, consumes 250W. In the quest for more efficient hardware for deep learning, biology is a not a bad place to start looking.

The “neurons” used in deep learning are so-named because of their loose correspondence to biological neurons. There are however, a number of fundamental differences between the types of neurons used in deep learning and those we observe in biology [Crick, 1989]. Among them are:

1. Biological Neurons do not do Backpropagation: Neurons used in deep learning emit two types of signals - an activation on the forward pass, and a gradient on the backward pass. Biological neurons send signals down a one-way signalling pathway called an axon. They appear to lack any secondary signalling mechanism for sending gradient backwards.

2. Biological Neurons communicate with Spikes: Neurons in deep learning have continuous, differentiable activation functions. This is necessary in order to propagate useful gradients back through the network. Biological neurons are best understood as dynamical systems, which output streams of all-or-nothing signals called “spikes”, which are some function of recent inputs to the neuron.

These two characteristics pose a conundrum to those looking to reconcile theories in machine-learning with how the brain might be reasonably expected to operate. The recent successes in deep learning have been based on achieving gradient-descent by propagating error-gradients backwards through a network. But it is not clear at all how biological neurons could achieve this.

To address the “no biological backprop” problem, Scellier and Bengio [2017] proposed Equilibrium Propagation. This showed how one may propagate gradients through a deep network in a setting where neurons only produce one type of signal - the forward activation. The
authors use a continuous Hopfield network [Hopfield, 1984] - a symmetrically-weighted neural network whose dynamics are defined according to the gradient of an energy function \( \frac{\partial}{\partial s} \propto -\frac{\partial E}{\partial s} \), where \( s \) is the state of the neurons. Learning is based on allowing the network to converge to a fixed-point conditioned on the input data, then perturbing the output units towards the target, letting the network settle again, and then updating parameters to minimize a contrastive loss between the original fixed-point state and the perturbed fixed-point. Their work showed a semi-plausible mechanism by which biological neural networks (or artificial networks implemented as analog circuits) may be able to achieve gradient descent.

The original formulation of Equilibrium Propagation, however, still assumes continuous-valued units. In this paper, we constrain neurons to emit binary-valued signals, and look at how neurons can efficiently convey their real-valued activations to other neurons despite this bottleneck. Specifically, we show how a network of neurons can efficiently minimize an energy function when neurons are “spiking” - i.e. constrained to only communicate binary values at each time-step.

This line of research may be of interest for designing the next generation of neural network hardware. A continuous-dynamical system can be implemented with an analog circuits, but electrical issues such as capacitance, inductance, and cross-talk make it difficult to faithfully transmit analog values over a circuit. Digital signals, by comparison, can be transmitted with ease. The brain appears to use a hybrid approach, with neurons having analog internal dynamics but communicating with one another using digital “spikes”.

2 Background

2.1 A Neural Network as a Dynamical System

Suppose we have a network of recurrently connected neurons with symmetric weights \( w_{ij} = w_{ji} \). This is known as a continuous Hopfield Network. Hopfield [1984] proposed an energy-function for such a network, which can be defined as:

\[
E(s) = \frac{1}{2} \sum_i s_i^2 - \sum_{i \neq j} w_{ij} \rho(s_i) \rho(s_j) - \sum_i b_i \rho(s_i) \tag{1}
\]

Where \( s_i \) is the activation of neuron \( i \), \( w_{ij} \) and \( b_i \) are model parameters, and \( \rho \) is a nonlinearity. Scellier and Bengio [2017] use a hard sigmoid function: \( \rho(s) = [s]_a^b \), where \([:]_a^b\) indicates that values outside the range of \( a \) and \( b \) are clipped to these limits. Given this energy function, we can define the temporal dynamics that minimize this energy with respect to activations:

\[
\frac{\partial s_j}{\partial t} = -\frac{\partial E(s_j)}{\partial s_j} = -s_j + \rho'(s_j) \left( \sum_i w_{ij} \rho(s_i) + b_j \right) \tag{2}
\]

Where \( \rho'(s_j) \) is the derivative of the activation function about \( s_j \). For implementation in discrete time, this can be expressed as a difference-equation (this is known as the Forward Euler Method):

\[
s_j^t = \left[ (1 - \epsilon) s_j^{t-1} + \epsilon \rho'(s_j^{t-1}) \left( \sum_i w_{ij} \rho(s_i^{t-1}) + b_j \right) \right]_0^1 \tag{3}
\]

Where \([:]_0^1\) indicates clipping to range \([0, 1]\) and \( \epsilon \in (0, 1) \) can be seen either as the size of the time-step or as the learning-rate of the activations. This update will converge to the optimum for a sufficiently small \( \epsilon \) (e.g. \( \epsilon = \frac{1}{2} \)).

2.2 Equilibrium Propagation

Scellier and Bengio [2017] proposed a method for using a continuous Hopfield Network to implement gradient descent on a loss defined over a subset of units in the network. They propose a two-phase learning algorithm called Equilibrium Propagation. In Equilibrium Propagation, units are partitioned into input, hidden, and output neurons, whose states we denote \( s_{in}, s_{hid}, \) and \( s_{out} \), respectively. They define some loss function between some target variable \( y \) and output activations:

\[
C(s_{out}, y)
\]

In the “Negative Phase”, we are given an input vector \( x \), and clamp the corresponding input units to that value: \( \langle s_{in} = x \rangle \). The remaining units \( (s_{hid} \) and \( s_{out} \)) are allowed to settle to an energy minimum \( s^- \) according to Equation 3.

In the “Positive Phase”, the output units are “weakly clamped” by the loss function. The “weak clamping” is done by adding the loss to the energy function from Equation 1: \( E^\beta(s) = E(s) + \beta C(s_{out}, y) \) (where \( \beta \) is some small scalar), and allowing the network to briefly settle to a state \( s^+ \). Finally, network parameters are updated according to the difference between these states:

\[
\Delta w = \eta \left( \frac{\partial E(s^+)}{\partial w} - \frac{\partial E(s^-)}{\partial w} \right) \approx -\frac{\partial C(s_{out}, y)}{\partial w} \tag{4}
\]

Where \( \eta \) is some learning rate. Scellier and Bengio [2017] show that for small \( \beta \), the resulting parameter
3 Binary Communication

Suppose we now operate under the constraint that neurons can only output binary values at each time-step. Our objective is to optimally converge to the same fixed-points as the continuous-valued dynamical system, under the constraint of binary communication between neurons. In other words, we constrain our neurons to obey the interface:

\[ q^t_j, s^t_j, z^t_j = f(q^{t-1}_j, s^{t-1}_j, w_{j,j}, b_j, z^{t-1}_j) \] (5)

Where \( q^t_j \in \{0, 1\} \) is the binary output of neuron \( j \), \( q_{j,j} \in \{0, 1\}^D \) are the binary signals of other neurons in the network, \( s^t_j \in \mathbb{R} \) is the external state associated with a neuron, \( w_{j,j}, b_j \) are the parameters associated with neuron \( j \), and \( z^t_j \) is the internal state of encoders and decoders which we will discuss in the following section. Note that the only values that are communicated between neurons are the binary \( q^t_j \)'s. Our goal is to design our neurons so that despite being limited by binary communication, the states \( s \) in our network to converge to the same fixed point as they would when following the real-valued dynamics of Equation 6.

We propose to design our neurons as follows:

\[
\begin{align*}
    u^t_j &= \sum_i w_{ij} q^{t-1}_i \\
    v^t_j, z^t_{\text{dec},j} &= \text{dec}(u^t_j, s^{t-1}_{\text{dec},j}) \\
    \epsilon^t_j, z^t_{\text{anneal},j} &= \text{anneal}(\epsilon^{t-1}_j, v^t_j, z^{t-1}_{\text{anneal},j}) \\
    s^t_j &= [(1 - \epsilon^t_j) s^{t-1}_j + \epsilon^t_j \rho'(s^{t-1}_j) (v^t_j + b_j)]_0^1 \\
    q^t_j, z^t_{\text{enc},j} &= \text{enc}(\rho(s^t_j), z^{t-1}_{\text{enc},j})
\end{align*}
\] (6)

Where \( \text{enc} \) and \( \text{dec} \) are functions for encoding and decoding signals between neurons, \( \text{anneal} \) is a function of updating the step size \( \epsilon \), and the form of internal state variables \( z_j = (z_{\text{dec},j}, z_{\text{anneal},j}, z_{\text{enc},j}) \) will be defined in the following sections.

In this work we show how various definitions of \( \text{enc} \), \( \text{dec} \) and \( \text{anneal} \) affect the convergence of our discrete dynamics to the true minimum of the energy (Equation 1). In the following sections we propose a quantization method that allows our neurons to efficiently settle towards this fixed point.

3.1 Stochastic Approximation

One approach we could take is to look at this as a Stochastic Approximation problem from the perspective of each neuron. The task of Stochastic Approximation is to keep an online estimate \( \hat{\theta}^t \) of a time-varying parameter \( \theta^t \) from a stream of noisy samples \( x^t = \theta^t + \zeta^t \), where \( \zeta^t \) is some unbiased noise. When \( \theta^t \) is not constant in time, we stay the input is nonstationary.

Robbins and Monro [1951] showed that if the nonstationarity is transient (\( \theta^t \) converges to a final value over time), we can sequentially average out the noisy samples to form estimates:

\[ \hat{\theta}^t = (1 - \epsilon^t) \hat{\theta}^{t-1} + \epsilon^t x^t \] (7)

If we anneal the step-size (or learning rate) \( \epsilon^t \) in such a way that \( \sum_{t=0}^{\infty} \epsilon^t = \infty \) and \( \sum_{t=0}^{\infty} (\epsilon^t)^2 < \infty \), then our estimator eventually converges to the true parameter values (\( \lim_{t \to \infty} \hat{\theta}^t = \theta^t \)). For stationary problems, when \( \theta^t = \theta^0 \), \( \forall t \), the optimal annealing schedule is \( \epsilon^t = \frac{1}{t} \), which corresponds to a simple moving average. For nonstationary signals (e.g., the activations in our network, which undergo some transient dynamics before settling), we can converge faster by forgetting early samples, so that the average is not corrupted by stale values. There are a number of ways to do this [George and Powell, 2006]. A simple one is to schedule the step-size as:

\[ \epsilon^t = \frac{\epsilon^0}{(t)^\eta} \] (8)

With the exponent \( \eta \in (\frac{1}{2}, 1) \). This guarantees that as \( t \to \infty \), the inputs at \( t = 0 \) diminish to have zero weight relative to the most recent inputs, but the average still smooths over an ever-growing number of samples.

3.2 A Naive Approach: Stochastic Rounding and the Robinson-Munroe Annealing

In our case, the “true” parameter \( \theta \) corresponds to the total pressure exerted on neuron \( j \) by the rest of the network: \( \rho'(s^{t-1}_j) \left( \sum_i w_{ij} \rho(s^{t-1}_i) + b_j \right) \) (from Equation 3). The noise arises from trying to represent real signals with a temporal stream of bits. The nonstationarity arises from the fact that the rest of the network has not yet settled to the fixed point. Note that our estimate itself affects future inputs: Neurons are connected recurrently in a network and the estimator in neuron \( i \) affects the estimator in neuron \( j \) which in turn affects the estimators in neuron \( i \).
Suppose each input neuron \( i \) in Equation 6 stochastically outputs bits \( q_i^t \sim \text{Bernoulli}(\rho(s_i^t)) \), where \( \rho(s_i) \in (0,1) \) is the neuron’s activation. Since \( q_i^t \) is an unbiased estimator of \( \rho(s_i) \), a neuron \( j \) receiving this signal should eventually average it out, along with all its other inputs, to achieve a correct estimate of \( \rho'(s_j^{t-1}) (\sum w_{ij} \rho(s_i^{t-1}) + b_j) \), provided that its input neurons do indeed converge to the correct fixed point \( s_j^\tau \). A simple communication scheme can then be described (with reference to the variables in Equation 6) as:

\[
\begin{align*}
q^t &= \text{Bern}(\rho(s^t)) \quad \text{Stochastic Encoder} \quad (9) \\
v^t &= u^t \quad \text{Identity Decoder} \quad (10) \\
\epsilon^t &= \frac{1}{(t)^n} \quad \text{Annealer} \quad (11)
\end{align*}
\]

### 3.3 Better Averaging with Adaptive Step Sizes

In choosing the step-size for stochastic optimization, we face a trade-off. Small step sizes allow us to average out noise, but also cause our current estimates to include outdated values of the time-varying parameter \( \theta^t \). It can therefore be advantageous to adaptively adjust our step size according to our estimate of how nonstationary \( \theta \) is. George and Powell [2006] review several existing step-size adaptation algorithms and propose one of their own called Optimal Step-Size Adaptation (OSA) which, similarly to a Kalman filter, adjusts its step-size according to the ratio of the estimated drift in the underlying parameter and the noise in the measurement. OSA is “optimal” in the sense that it optimally estimates the parameter \( \theta \) if the drift and noise are known. Since they are not - OSA also estimates these quantities, and bases the step-size on these estimates. OSA has only a single parameter, \( \bar{\nu} \), which is the target learning rate for estimating the drift and noise. The full algorithm is included in Appendix A.

### 3.4 Better Encoding with Sigma-Delta Modulation

There are more efficient ways to communicate a time-varying real value than to send random bits centered around that value. A simple method from signal processing for encoding time-varying signals is Sigma-Delta modulation [Candy and Temes, 1962]. Suppose we have a time-varying input signal \( x_1, \ldots, x_T \) where \( x_t \in (0, 1) \forall t \). We then quantize \( x_t \) into \( q_t \) according to:

\[
\phi' = \phi'^{-1} + x^t \\
q^0 = \left\lfloor \frac{\phi'}{2} \right\rfloor \quad \text{Sigma Delta Encoder} \quad (12) \\
\phi' = \phi' - q^t
\]

Where \([a > b]\) evaluates to 1 if \( a > b \) and 0 otherwise. By expanding Equation 12 recursively, we can verify that if \( x^t \in (0, 1) \) and \( \phi_0 = 0 \), the mean quantization error is bounded: \( \frac{1}{T} \sum_{t=0}^T (x^t - q^t) \leq \frac{1}{2T} \). So we have \( O(1/T) \) convergence, compared to the \( O(1/\sqrt{T}) \) convergence that we would get from averaging out a stochastic estimator.

Note that this corresponds to an “integrate-and-fire” quantization - inputs are added to a “potential” \( \phi \), and once that potential crosses a threshold a “spike” \( (q(t) = 1) \) is sent out, and subtracted from the potential. Sigma-Delta modulation has previously been used as a model of the neural spiking mechanism: [Yoon, 2016], Zambrano and Bohte [2016], O’Connor et al. [2017].

### 3.5 Better Bit-Economy with Predictive Coding

When the signal is time-varying, it seems like a poor use of bandwidth to simply communicate a stream of bits that averages out to the current signal value. Instead, we can use an encoding scheme wherein neurons primarily send temporal changes in the signal value to downstream neurons, and downstream neurons integrate these changes. This is an instance of Predictive Coding, a widely used concept in the Signal Processing literature. Predictive Coding has in the past been proposed as a possible mechanism in neural communication. [Srinivasan et al., 1982], [Shin, 2001], [Tewksbury and Hallock, 1978], [Bharioke and Chklovskii, 2015].

Lossy Predictive Coding is a method for efficiently encoding a real-valued signal as a bitstream, and decoding it again on the other end of a communication channel. At each time-step, a predictor attempts to predict the current signal from past signal values, and the prediction is subtracted from the signal before quantization. On the receiving end, the same predictor is used to reconstruct the signal from the stream of bits. In the case where the predictor is a linear function of past inputs, we can exploit the commutativity of the weight-multiplication and decoding operations [O’Connor et al., 2017] to sandwich a weight matrix between the encoders and decoders. Here, we formulate an extremely simple predictor \( \text{Pred}(x^{-1}, \ldots, x^0) = (1 - \lambda)x^t \) where \( \lambda \in (0, 1) \). We write our encoder (with reference to the variables in Equation 6) as:

\[
\begin{align*}
\phi' &= \phi'^{-1} + x^t \\
q^t &= \left\lfloor \frac{\phi'}{2} \right\rfloor \quad \text{Sigma Delta Encoder} \quad (12) \\
\phi' &= \phi' - q^t
\end{align*}
\]
\[
a^t = \frac{1}{\lambda}(s^t) - (1 - \lambda)\rho(s^{t-1}) \quad \text{Predictive Encoder}
\]
\[
q^t = Q(a^t)
\]

Where \(Q\) is some (possibly stateful) quantization procedure, such as Sigma-Delta modulation (Equation 12) or Stochastic Rounding (Equation 9). On the decoding side, we sum up the weighted quantized inputs and invert the encoding function:
\[
u_j^t = \sum_i w_{ij}q_i^{t-1}
\]
\[
v_j^t = (1 - \lambda)v_j^{t-1} + \lambda u_j^t \quad \text{Predictive Decoder}
\]

When \(\lambda\) is close to 0, we have a system that only sends changes in state, and accumulates these changes in a running sum. When \(\lambda\) is 1, we recover the case with no predictive coding.

### 3.6 Lambda-Annealing

As was the case with \(\epsilon\), it is also possible to anneal the prediction-factor \(\lambda\). Intuitively, we would like to start the convergence process with a very short memory (\(\lambda\) close to 1), primarily using bits to communicate the rapidly changing current state. Later, as we approach a fixed point, we would like to lengthen the memory (\(\lambda\) close to 0) and use our bits to communicate increasingly fine increments to the state.

### 3.7 The Resulting Model

Combining Sigma-Delta encoding from Equation 12 with the predictive encoder/decoder of Equations 13 and 14 by plugging them all into Equation 6 results in a biologically-plausible model that applies double-exponential smoothing to inputs and produces output spikes with an integrate-and-fire mechanism:
\[
v_j^t = (1 - \lambda^t)v_j^{t-1} + \lambda^t \sum_i w_{ij}q_i^{t-1}
\]
\[
s_j^t = [(1 - \epsilon^t)s_j^{t-1} + \epsilon^t \rho(s_j^{t-1}) (v_j^t + b_j) - 1]
\]
\[
a^t = \frac{1}{\lambda^t}(s^t) - (1 - \lambda^t)\rho(s^{t-1})
\]
\[
q^t_j = [q_j^{t-1} + a_j^t > \frac{1}{2}]
\]
\[
\phi^t_j = \phi_j^{t-1} + a_j^t - q^t_j
\]

Figure 1 shows some example dynamics from our model.

### 4 Experiments

We explore several combinations of the hyperparameters \(\epsilon^t, \lambda^t\), introduced in Section 3. First in Section 4.1, we compare the rate at which these various hyperparameter settings converge to the fixed point for randomly initialized networks. Then in Section 4.2 we apply the more promising settings to train a neural network on the MNIST dataset.

#### 4.1 Convergence

To understand how our encoding/decoding parameters affect the rate of convergence, we use a randomly initialized network with 3 layers of [500-500-10] units, where the first is considered the "input" layer and is clamped to a random input vector \((s_{in} = x)\). We simulate the two-phase learning of Equilibrium Propagation by running the network for a fixed number of steps.
Figure 2: A network is presented with a constant input at \( t = 0 \), and allowed to settle. Then at \( t = 100 \) the output layer is perturbed, and the network is allowed to settle to the new fixed point. The \( y \) axis indicates the log-mean-error between the true fixed-point \( s^{\text{fixed}} \), and the current state of \( s \) of the quantized network. \( s^{\text{fixed}} \) is calculated by running a continuous-valued network (with the same parameters and input) to convergence. Note that \( s^{\text{fixed}} \) is different for \( t < 100 \) and \( t \geq 100 \) due to the external perturbation at \( t = 100 \). Shaded regions indicate the standard deviation over 20 runs with randomly initialized networks.

In order to reach similar performance to the continuous-valued network, we had to extend the positive and negative phases to (100, 50) steps respectively, compared to the (20, 4) steps used in real-valued equilibrium propagation. We found no significant difference between the networks trained with OSA and with annealing schedules (after finding the optimal annealing-parameters for each model with a Gaussian-Process parameter search - see Appendix C). In the remainder of this section, we report the results for the OSA model with a constant \( \lambda = 0.275 \) predictive-coding coefficient. Our binary-network performed similarly on the test set to the continuous-valued-network (see Figure 3), achieving a (2.37% test / 0.15% training) error, compared to the continuous network’s (2.51% test / 0.27% training) error.

We also ran our model on a deeper network with 3 hidden layers [784-500-500-500-10], and found that our network slightly underperformed the continuous-valued network, achieving (3.65% test / 3.02% training) error vs (2.42% test / 0.27% training) error for the continuous-valued network. The discrepancy is likely due to the quantized network needing longer negative/positive convergence phases. The learning curves and details on the parameterizations of these experiments can be found in Appendix C.
5 Discussion and Related Work

Much of the work in the stochastic approximation literature is about how to adapt step-sizes according to the statistics of the incoming sample stream [Chau and Fu, 2015], [George and Powell, 2006]. It is unclear whether we can transfer adaptive step-size algorithms to the machine learning task. It is unclear if this approach would scale to a more standard problem, so that the network reaches the correct fixed point in the end, but this needs more work. [Bharioke and Chklovskii, 2015] suggested that including a non-linearity in the predictor can have the effect of rapid online adaptation of prediction coefficients. Adaptive predictive coding could allow us to perform efficient inference on nonstationary data. We can imagine constructing a network where neurons use their bits to communicate fine changes in state when the network is near a fixed point but then adapts itself to take larger, coarser steps when it sees the input has started changing rapidly (e.g. during a saccade).

Mesnard et al. [2016] also implemented Equilibrium Propagation with spiking neurons. Their model was primarily built to mimic the leaky-integrate-and-fire dynamics of biological neurons. There was no annealing and their neurons do not converge to a fixed point when presented with a constant input. They demonstrate that the model can train on a toy dataset, but it is not clear if this approach would scale to a more standard machine learning task.

There are still several obstacles to doing truly biologically plausible deep learning. One subtle issue is that we rely on “capturing” a negative state $s^-$ and a positive state $s^+$ in order to do the parameter update (Equation 4). This requires holding onto two states at once - something which biological neurons seem unlikely to do. If we instead take the approach of using the rate of change of the postsynaptic neuron at the beginning of the positive phase, as suggested in Bengio et al. [2015], Scellier and Bengio [2017], (i.e. $\Delta w_{ij} \propto \rho(s_i \frac{ds_i}{dt})$) we have the problem that we get very noisy updates due to the quantization.

Another lingering biological-implausibility that is not specific to our algorithm is that we still use symmetric weights. Learning with symmetric weights implies an additional communication channel to synchronize synapse $w_{ij}$ of neuron $j$ to synapse $w_{ji}$ of neuron $i$. However recent work by [Scellier et al., 2018] and Lillicrap et al. [2014] seems to suggest that this may not be a problem, because weights tend to align themselves to be approximately symmetrical through learning anyway. Another obstacle is that biological networks do not appear to have distinct forward/backward passes, or negative/positive phases (except perhaps on the very slow timescale of the sleep/wake cycle). It is still not clear how one could do learning in a setting where new data is continuously coming in and we do not have the luxury of pausing our sensory input while we wait for our brains to do a forward/backward pass or settle to an energy minimum. Even if we could, we face the problem of Catastrophic Forgetting, wherein deep networks tend to forget old training data when presented with a nonstationary stream of training samples (though Kirkpatrick et al. [2017] have done some work addressing this). Finally the question of how to learn temporal sequences without doing backpropagation-through-time remains an open one, though recent works such as Olivier et al. [2015] and Tallec and Ollivier [2017] have begun to address this.

6 Conclusion

We demonstrate that we can train a network with Equilibrium Propagation even when neurons are constrained to only communicate binary values. To achieve efficient communication between neurons, we use ideas from Stochastic Approximation and Predictive Coding.

We believe that this work is relevant to designing of the next generation of neural computing hardware. In modern computers, most of the energy cost is not spent on computation (in terms of adds and multiples), but in moving data around Horowitz [2014]. It seems likely that future neural computing hardware will consist of neurons implemented as physical circuits, with computation co-located with memory, so that parameter values never need to be moved. The main energetic bottleneck will then be the communication between neurons. In the brain, Attwell and Laughlin [2001] estimate that 81% of metabolic energy is spent on sending signals between neurons. It makes sense then, that neurons should have evolved to use the minimum number of spikes to communicate what they need to communicate. If the brain is doing something similar to Equilibrium Propagation, then neurons compute by collectively trying to find the fixed point of a dynamical system. Our work addresses the question of how we can efficiently find this fixed point when there is a communication bottleneck between neurons.

Code is available at https://github.com/quva-lab/spiking-eprop
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